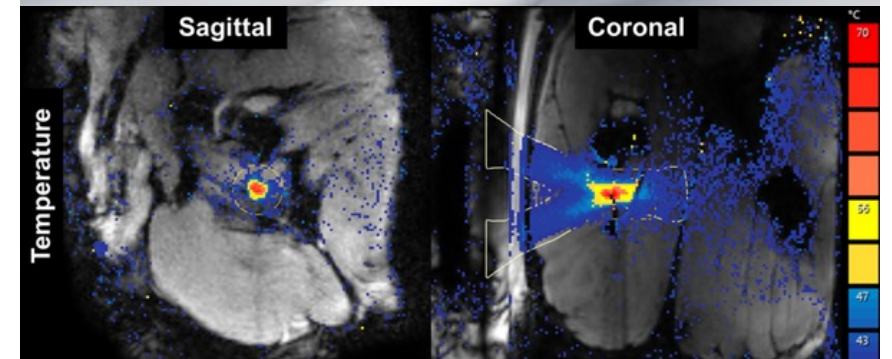
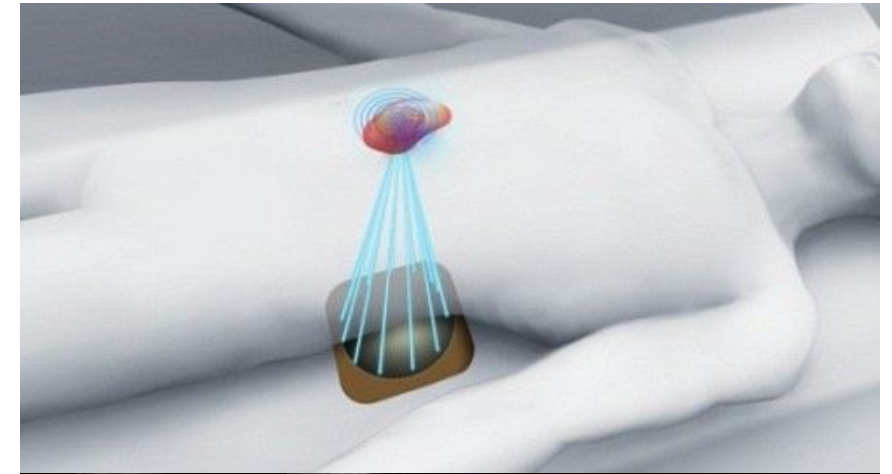
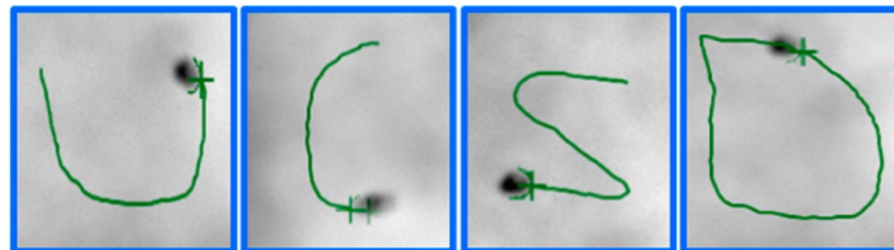
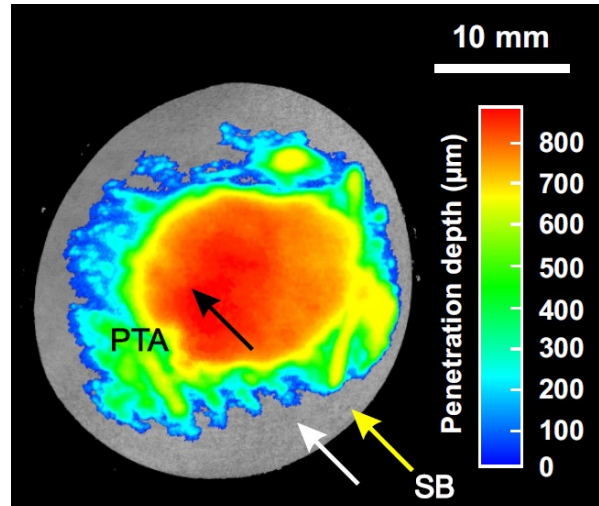


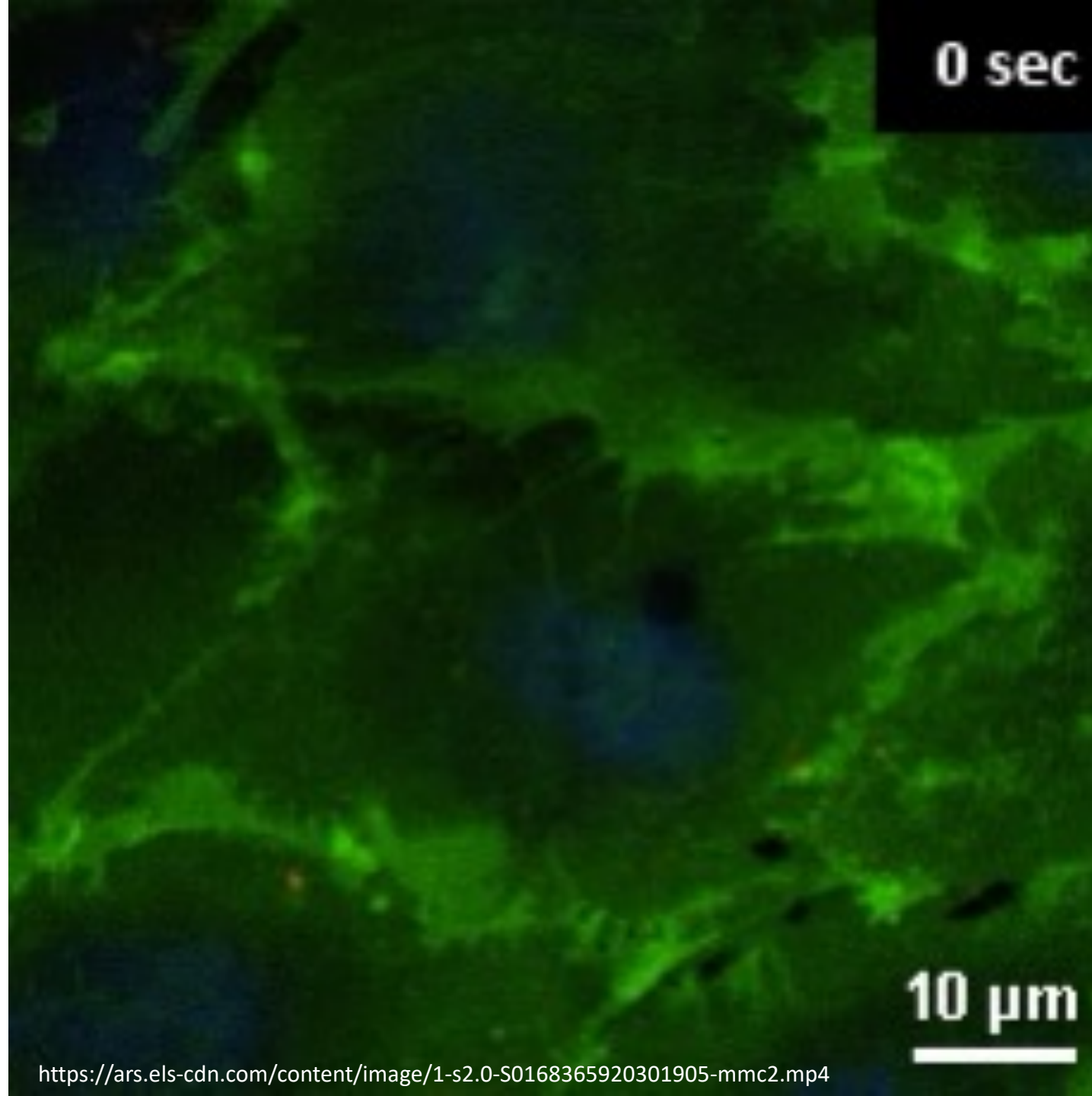
Biomedical Ultrasonics, 5 cr

Heikki Nieminen

13.9.-7.12.2023



Example:
sonoporation
in endothelial
cells





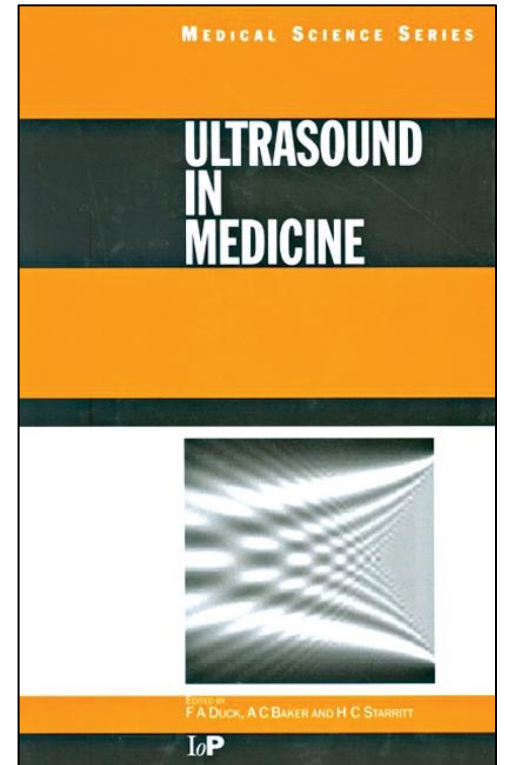
side view

General information

- Lectures: Heikki Nieminen
 - heikki.j.nieminen@aalto.fi, 050 501 9280
- Course coordination:
 - Exercises: Alex Drago-Gonzalez, alex.dragogonzalez@aalto.fi
 - Workshops: Contact persons to be shared later
- Contact: primarily through Discussion forum, secondarily by email
- Course web-site:
 - Course website: <https://mycourses.aalto.fi/course/view.php?id=39047>
 - The course materials will appear there.

General information

- Course dates: 13.9.-15.12.2023
- Course materials:
 - Lecture slides
 - Articles discussed during the lectures
 - Slides contain hyperlinks to the original article that you should be able to access inside Aalto. If article is for some reason not accessible, it can be provided separately on request.
 - Lecture notes will appear on course website
 - **Book: Duck et al: *Ultrasound in Medicine*, 1998**
- Further reading:
 - Kinsler et al: *Fundamentals of Acoustics*, 4th ed
 - Dowsett et al.: *The Physics of Diagnostic Imaging*, 2nd ed



Evaluation

- 5 credits course
- Evaluation is based on the following:
 - Exercises (0.30 weight) (Score: 1-5; 50% = 1, 95% = 5; 50% is the limit for passable)
 - Quizzes (0.20) (Score: 1-5; 50% = 1, 95% = 5; 50% is the limit for passable)
 - Presentation (0.10) (Score: 1-5)
 - Report (0.40) (includes material generated in workshops in the lab) (Score: 1-5)
- Each evaluated on scale 1-5 points and using the weights
- To pass the course, one needs to pass each sub-category
- There will be no final exam

Goals of the course

Learning outcomes:

- **After taking the course, the student is able to explain in writing and calculations:**
 - basic linear and non-linear ultrasound–matter interactions (acoustic radiation force, acoustic streaming, cavitation, shock waves)
 - physics of biomedical ultrasonic applications, e.g., ultrasound imaging, quantitative ultrasonics, ultrasonic therapeutics
 - physics of ultrasonic actuation of matter (e.g. drug, drug vehicle, gas bubble, cell, tissue, organs)
- **In addition, the student is able to read scientific literature on biomedical ultrasonic applications in linear and non-linear domain.**



“Ideology” of the course

Physics → Applications → Exercises → Lab-work

Contents of the course

1. Linear acoustics

- Basic physics of acoustics
- Ultrasound imaging principles
- Quantitative ultrasonics

2. Non-linear acoustics

- Basic high-intensity ultrasound (HIU) physics
- Acoustic radiation force
- Ultrasound streaming
- Cavitation
- Shock waves
- Permeabilization, cutting & disintegration

3. Thermal acoustics

- Heating

Schedule

Subject to change, always follow MyCourses for any updates

Biomedical Ultrasonics course schedule 2023							
	Monday	Tuesday	Wednesday	Thursday	Friday	Comments	Color codes
4.09-8.09							Lectures
11.09-15.09			12 to 14	12 to 14			Exercise
17.09-22.09			12 to 14	12 to 14			Free week
24.09-29.09			12 to 14	12 to 14			
2.10-6.10			12 to 14	12 to 14			
9.10-13.10			12 to 14	12 to 14			
16.10-20.10							
23.10-27.10			12 to 14	12 to 14			
30.10-3.11			12 to 14	12 to 14		Lab work (preliminary plan, TBD)	
6.11-10.11			12 to 14			Lab work (preliminary plan, TBD)	
13.11-17.11			12 to 14	12 to 14			
20.11-24.11			12 to 14				
27.11-1.12			12 to 14	12 to 14			
4.12-8.12			HOLIDAY				
11.12-15.12						DL on 7.12. to hand-in reports	
18.12-22.12							

Early ultrasonics

- Pyroelectric effect, early/mid 19th century
 - Electric potential (V) response to temperature change
- René Just Haüy and Antoine César Becquerel proposed in 19th century :
 - Mechanical stress → Electric charge
 - Unfortunately, the experiments were inconclusive
- Pierre and Jacques Curie 1880
 - Pressure applied to quartz crystals → voltage
- Paul Langevin's SONAR studies during WW I (20th century)
 - Quartz sandwich transducer for submarine detection (lethal to fish in US beam)



Lorentz, Einstein and Langevin in 1927

<http://www.ob-ultrasound.net/langevin.html>

→ **Modern ultrasonics**

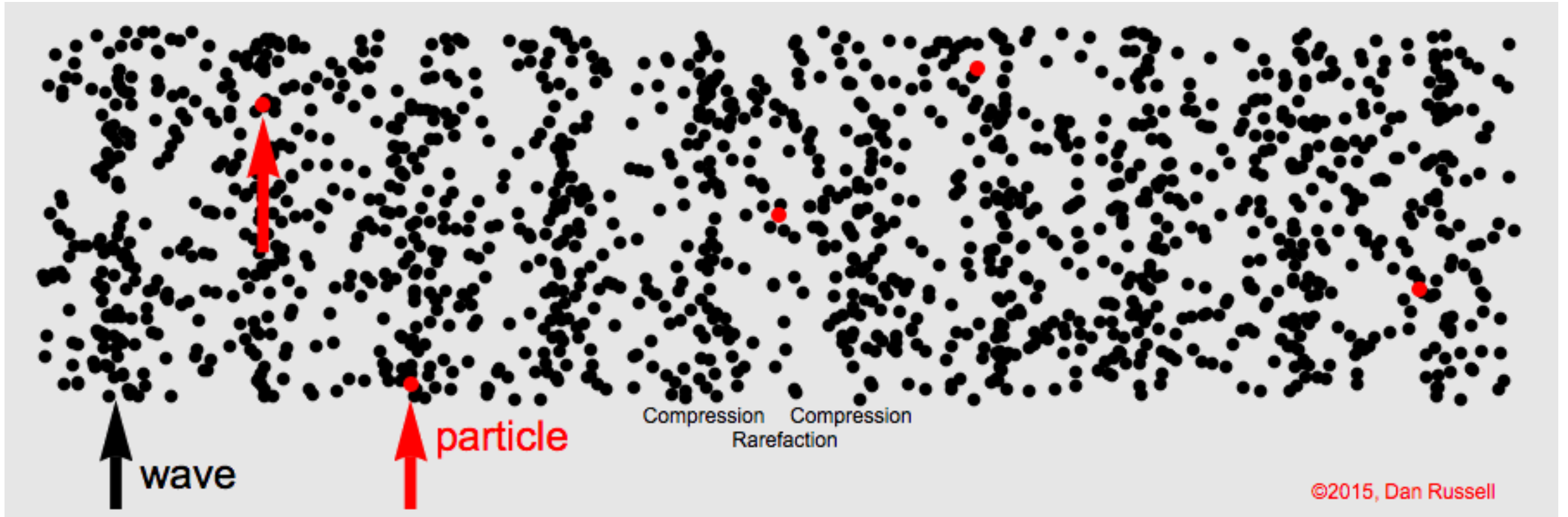
Why is ultrasound an attractive modality for biomedical applications?

- Allows non-destructive non-invasive non-touching **evaluation and actuation** of anatomy/physiology
- Approaches, e.g.:
 - Imaging
 - Quantitative characterization of pathologies and physiology
 - Ultrasonic actuation allows therapy and novel diagnostics based on actuation
- Non-ionizing
- Cheap imaging (vs. X-ray, CT, MRI, nuclear imaging)

Basic physics of acoustics

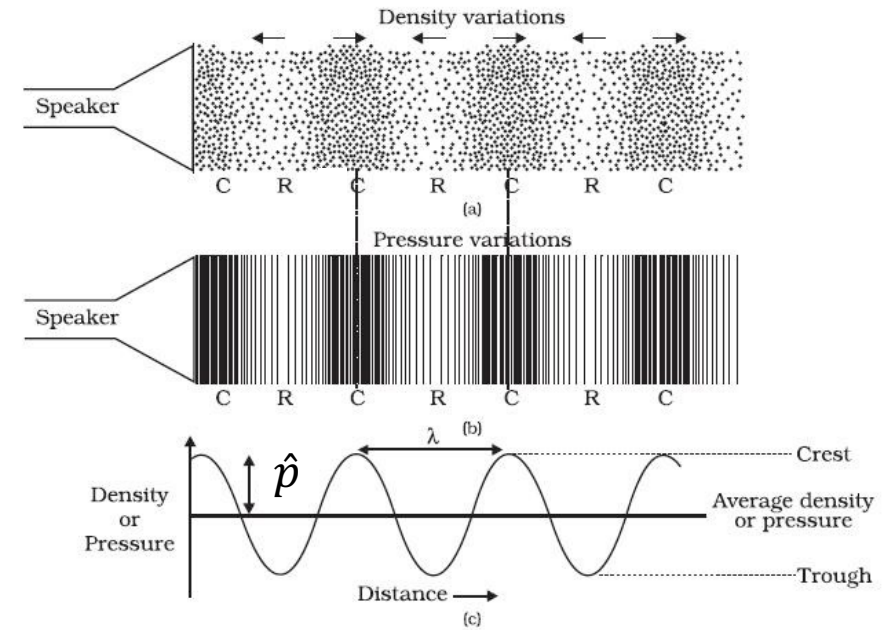
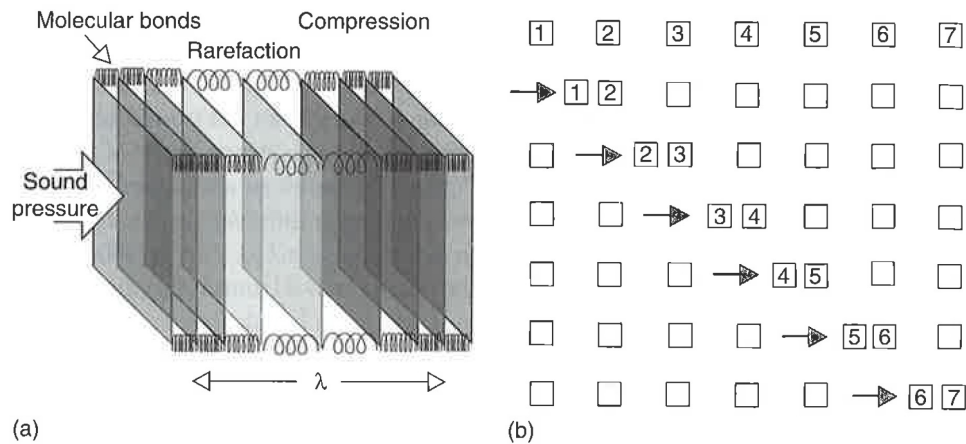
1. LINEAR ACOUSTICS

What is sound?



What is sound?

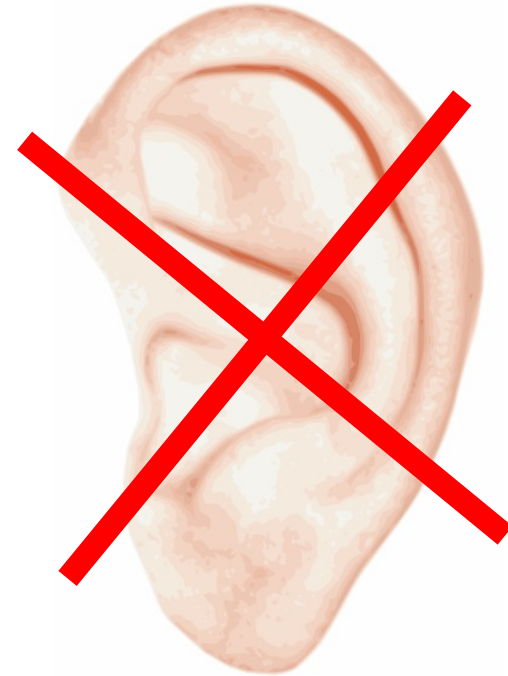
- Sound is a travelling density/pressure disturbance



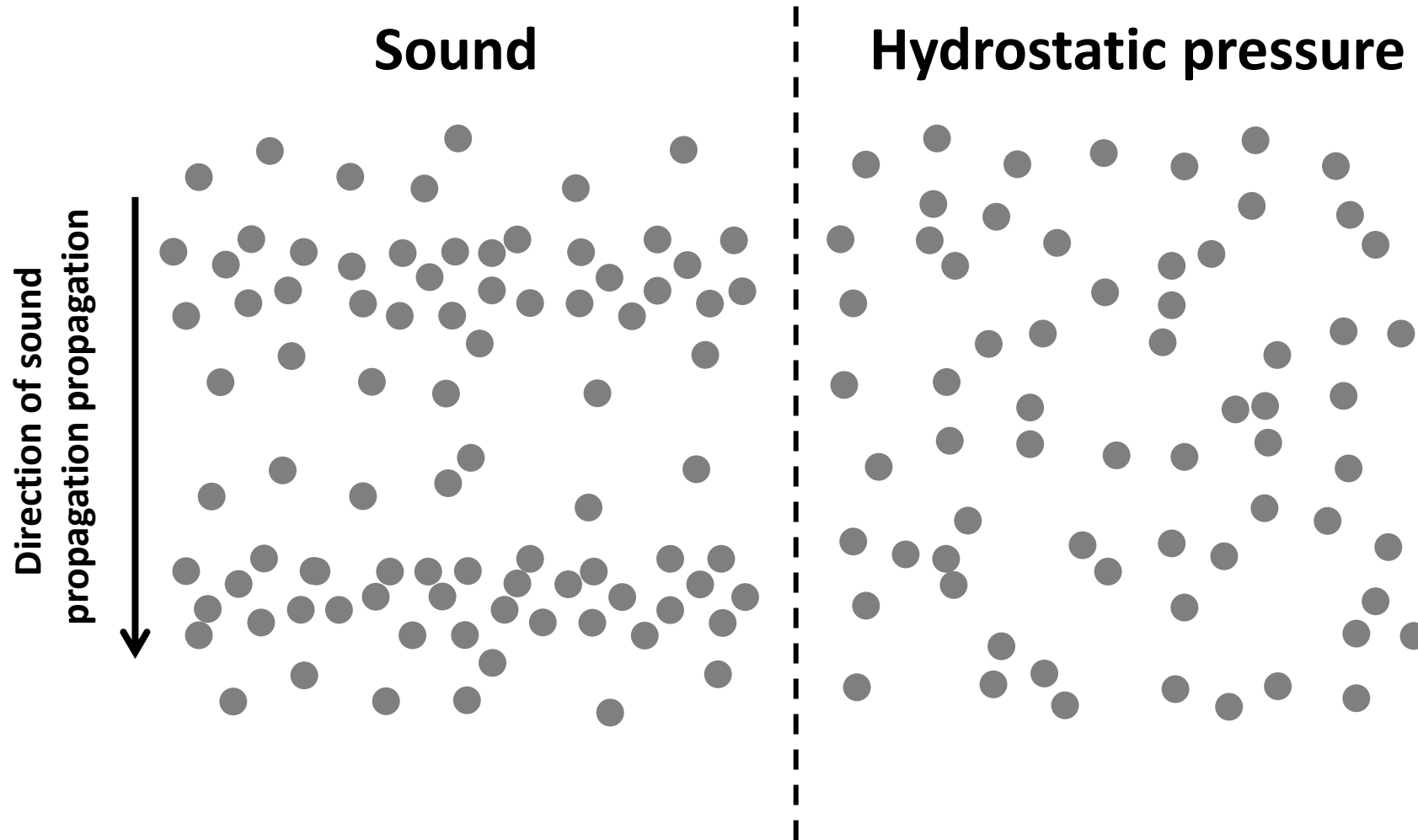
\hat{p} = pressure amplitude
 λ = wavelength

What is ultrasound?

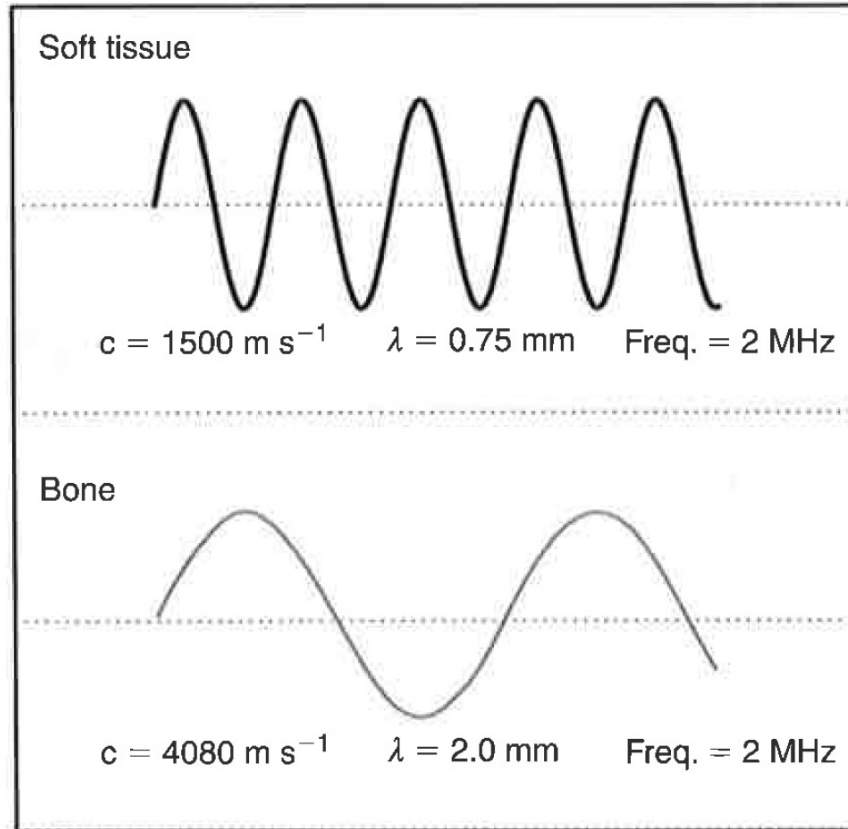
Ultrasound is a travelling density/pressure disturbance oscillating at a frequency > 20 kHz



Pressure vs. hydrostatic pressure



Wavelength



$$\lambda = \frac{c}{f}$$

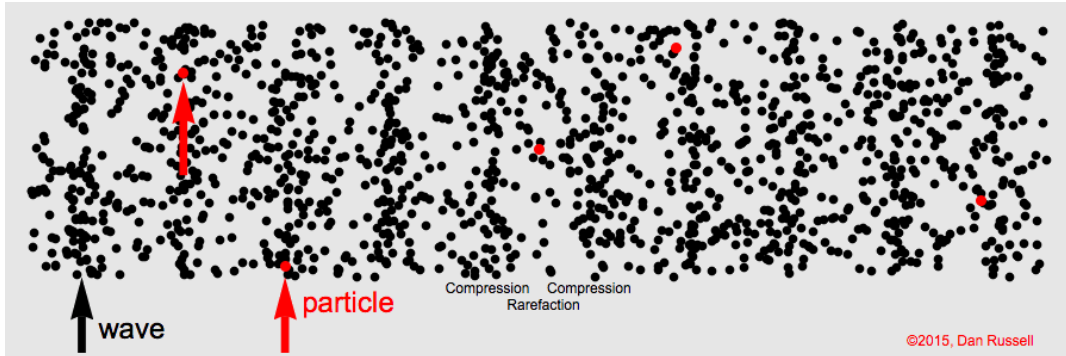
λ = wavelength
 c = speed of sound
 f = frequency

Wavelength

“Acoustically, soft tissue is very much like water.”

Pressure of sound

Longitudinal wave



p = complex pressure
 \hat{p} = peak pressure amplitude
 i = imaginary unit
 t = time
 x = position
 ρ_0 = density at rest
 Z = acoustic impedance

Pressure (sinusoidal Continuous wave):

$$\rightarrow \mathbf{p}_+ = \hat{p} e^{i(\omega t - kx)}$$

$$\leftarrow \mathbf{p}_- = \hat{p} e^{i(\omega t + kx)}$$

Real pressure:

$$\leftarrow p_- = \text{Re}\{\mathbf{p}_-\} = \hat{p} \cos(\omega t + kx)$$

$$\rightarrow p_+ = \text{Re}\{\mathbf{p}_+\} = \hat{p} \cos(\omega t - kx)$$

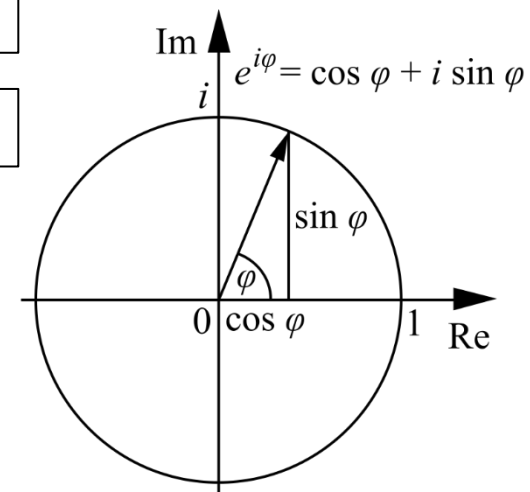
Wave number:

$$k = \frac{2\pi}{\lambda}$$

Association of pressure and particle velocity:

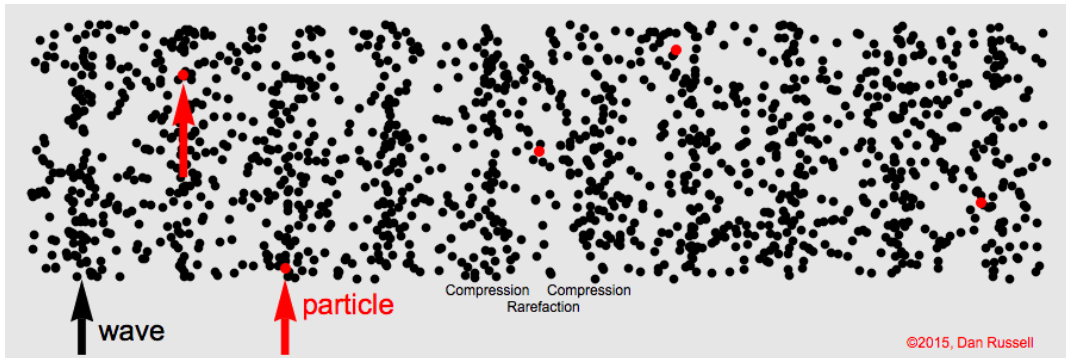
$$\rho_0 c = \frac{p}{u} = Z$$

$$p = \rho_0 c u = Z u$$



Particle velocity

Longitudinal wave



p = complex pressure
 \hat{u} = peak velocity
 i = imaginary unit
 t = time
 x = position

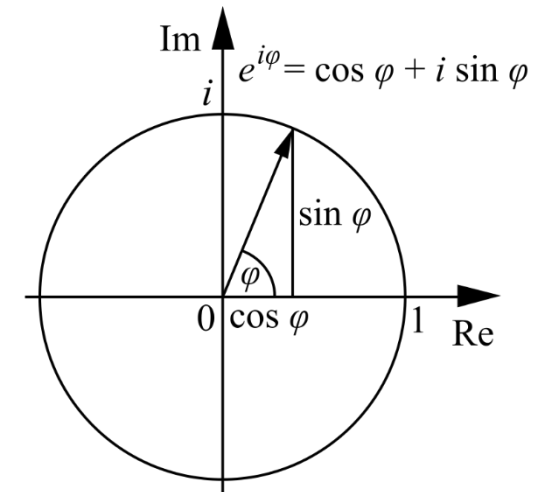
Particle velocity (sinusoidal continuous wave):

$$\mathbf{u}_+ = \frac{d\xi_+}{dt} = i\omega\hat{\xi}e^{i(\omega t - kx)} = \hat{u}e^{i(\omega t - kx)}$$

$$\mathbf{u}_- = \hat{u}e^{i(\omega t + kx)}$$

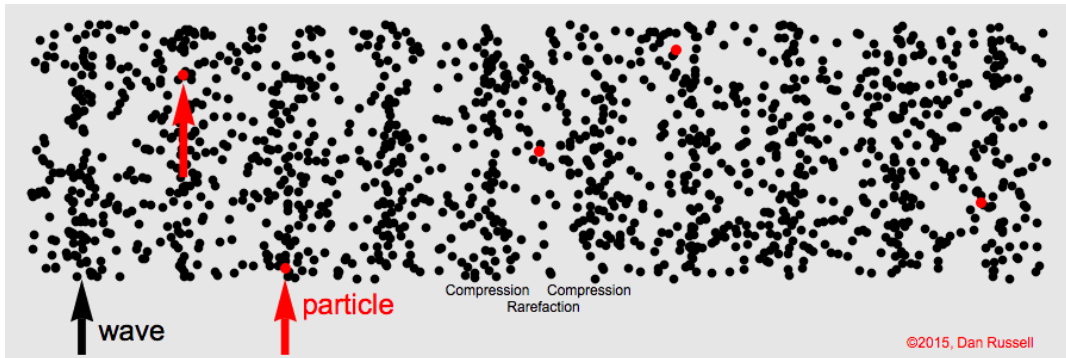
Real particle velocity:

$$u = \text{Re}\{\mathbf{u}\}$$



Particle displacement

Longitudinal wave



Particle displacement (sinusoidal continuous wave):

$$\xi_+ = \hat{\xi} e^{i(\omega t - kx)}$$

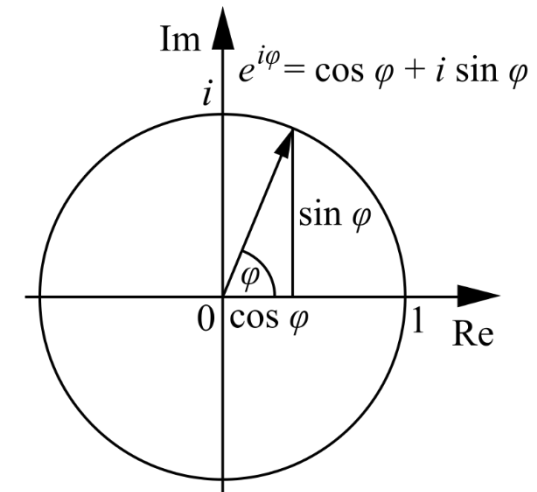
$$\xi_- = \hat{\xi} e^{i(\omega t + kx)}$$

Real displacement:

$$\xi = \text{Re}\{\xi\}$$



p = complex pressure
 $\hat{\xi}$ = peak displacement amplitude
 i = imaginary unit
 t = time
 x = position



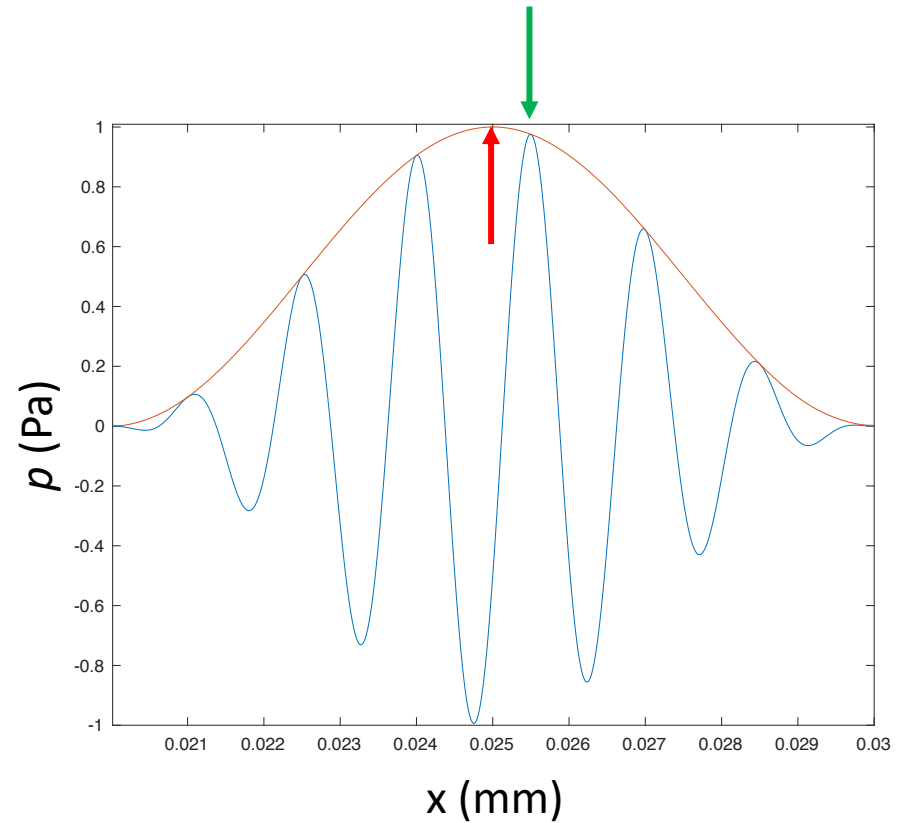
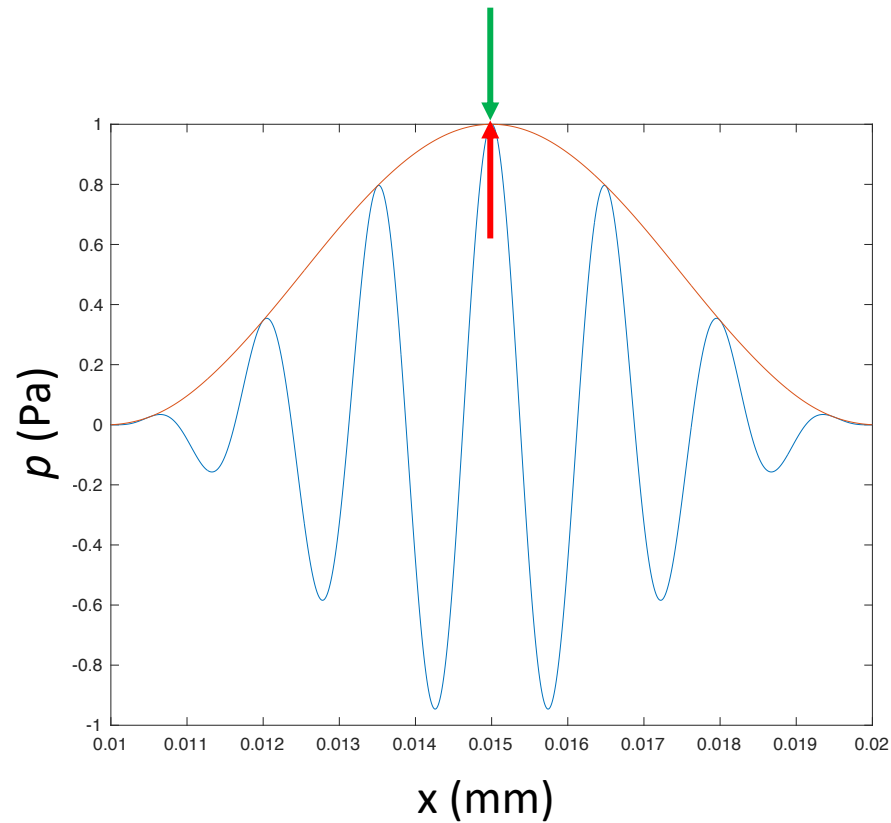
Intensity

- Intensity is describes the acoustic power of the ultrasound field per unit area
- Unit: W/m^2 or W/cm^2 (latter more commonly used in medical context)
- Instantaneous intensity:

$$I = \frac{p^2}{\rho_0 c}$$

Speed of sound

- Phase velocity
- Group velocity



Acoustic impedance

- A material property that describes how much *pressure* is generated in a medium from spatial displacement of its molecules at a given frequency. Sound is reflected at an interface between two materials with different acoustic impedances.

Acoustic impedance: $Z = \frac{p}{u} = \rho_0 c$

Unit: kg / sm² or Rayl

p = real pressure

u = particle velocity

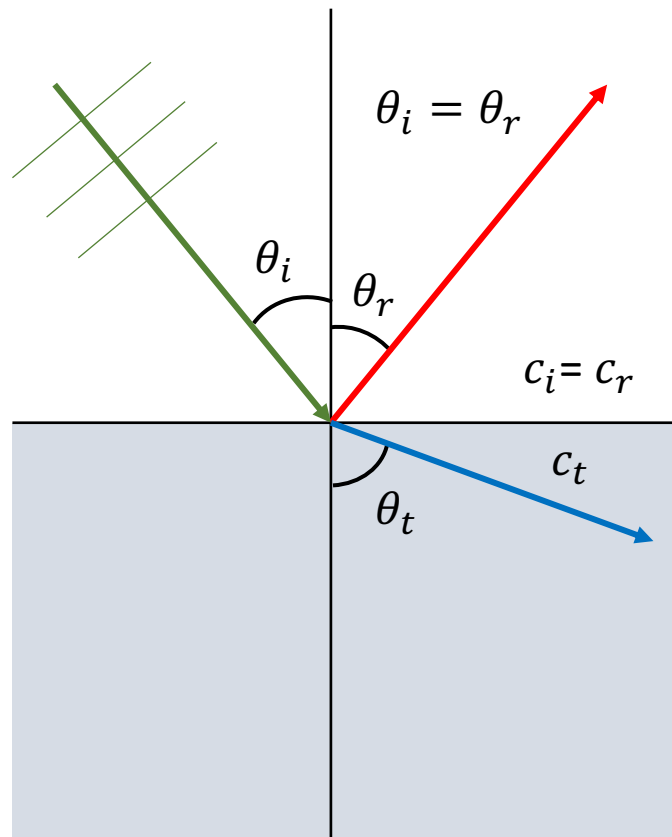
c = speed of sound

ρ_0 = density at rest

Acoustic impedance

Tissue or Material	Density (g/cm ³)	Speed of Sound (m/sec)	Acoustic Impedance [kg/(sec·m ²)] × 10 ⁶
Water	1	1480	1.48
Blood	1.055	1575	1.66
Fat	0.95	1450	1.38
Liver	1.06	1590	1.69
Kidney	1.05	1570	1.65
Brain	1.03	1550	1.60
Heart	1.045	1570	1.64
Muscle (along the fibers)	1.065	1575	1.68
Muscle (across the fibers)	1.065	1590	1.69
Skin	1.15	1730	1.99
Eye (lens)	1.04	1650	1.72
Eye (vitreous humor)	1.01	1525	1.54
Bone axial (longitudinal waves)	1.9	4080	7.75
Bone axial (shear waves)	1.9	2800	5.32
Teeth (dentine)	2.2	3600	7.92
Teeth (enamel)	2.9	5500	15.95

Reflection and transmission of a propagating wave



Snell's law:

$$\frac{\sin \theta_i}{c_i} = \frac{\sin \theta_t}{c_t}$$

i = incident

r = reflected

t = transmitted

Reflection and transmission coefficients of pressure

Reflection coefficient

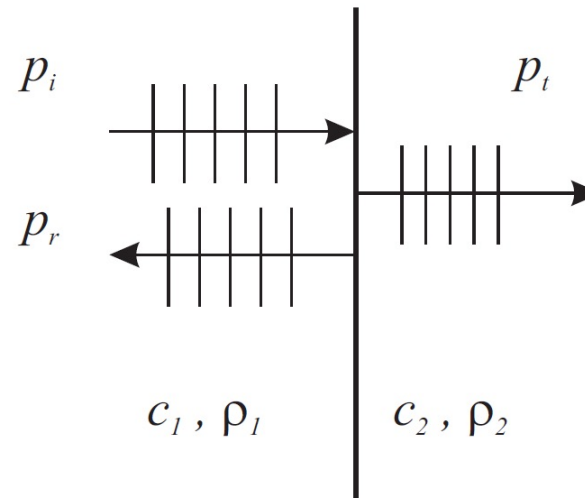
Applies to fluids

$$R = \frac{p_r}{p_i} = \frac{\rho_2 c_2 - \rho_1 c_1}{\rho_2 c_2 + \rho_1 c_1} = \frac{Z_2 - Z_1}{Z_2 + Z_1} = \frac{K_2/c_2 - K_1/c_1}{K_2/c_2 + K_1/c_1}$$

K = bulk modulus
 i = incident
 r = reflected
 t = transmitted

Transmission coefficient

$$T = \frac{p_t}{p_i}$$



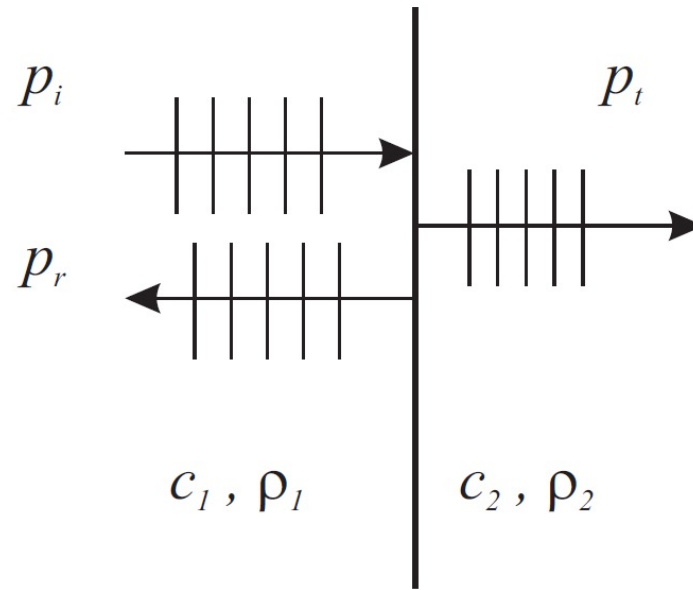
Reflection and transmission coefficient of intensity

Reflection coefficient

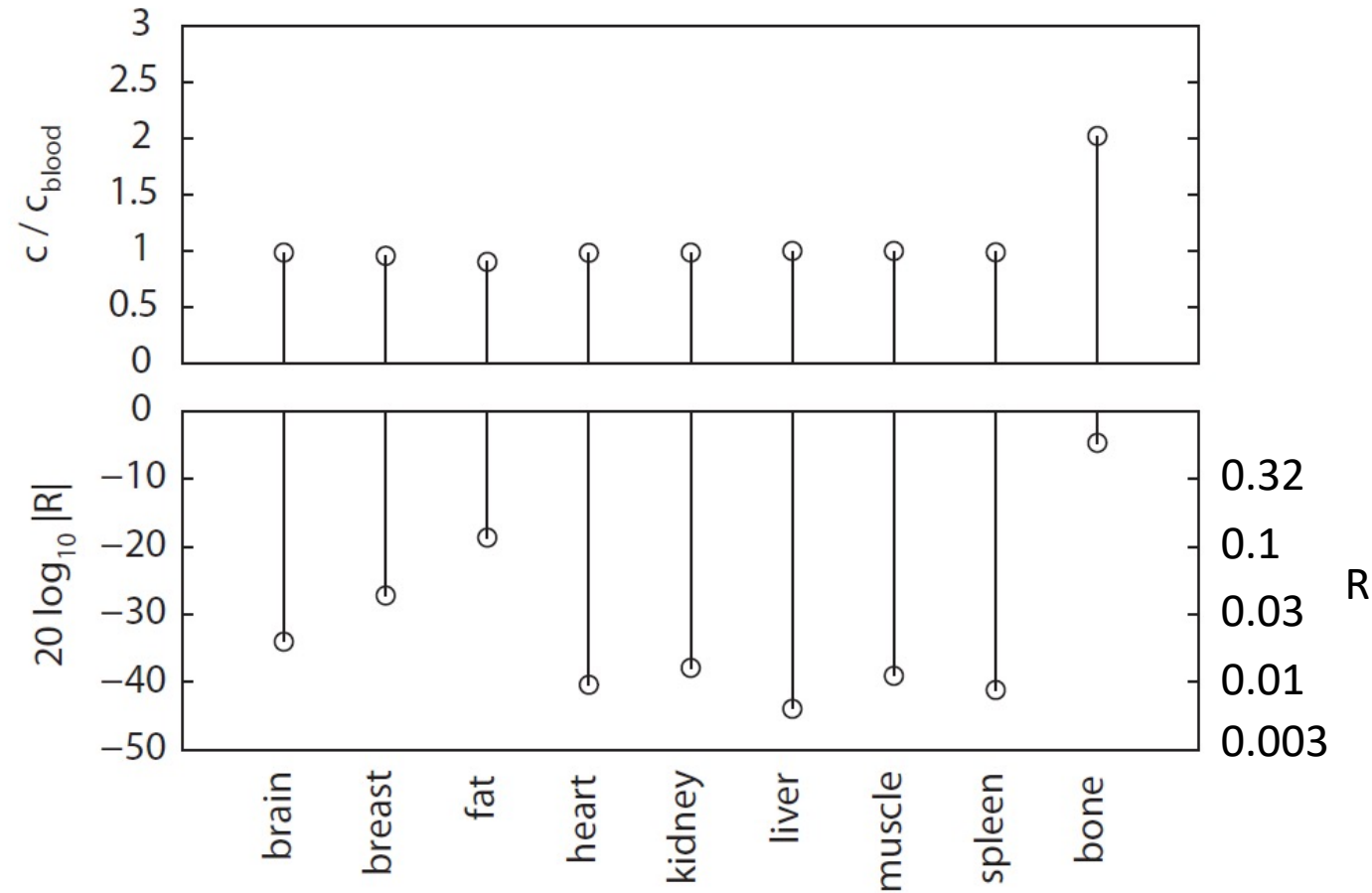
$$R_I = R^2 = \left(\frac{Z_2 - Z_1}{Z_2 + Z_1} \right)^2$$

Transmission coefficient

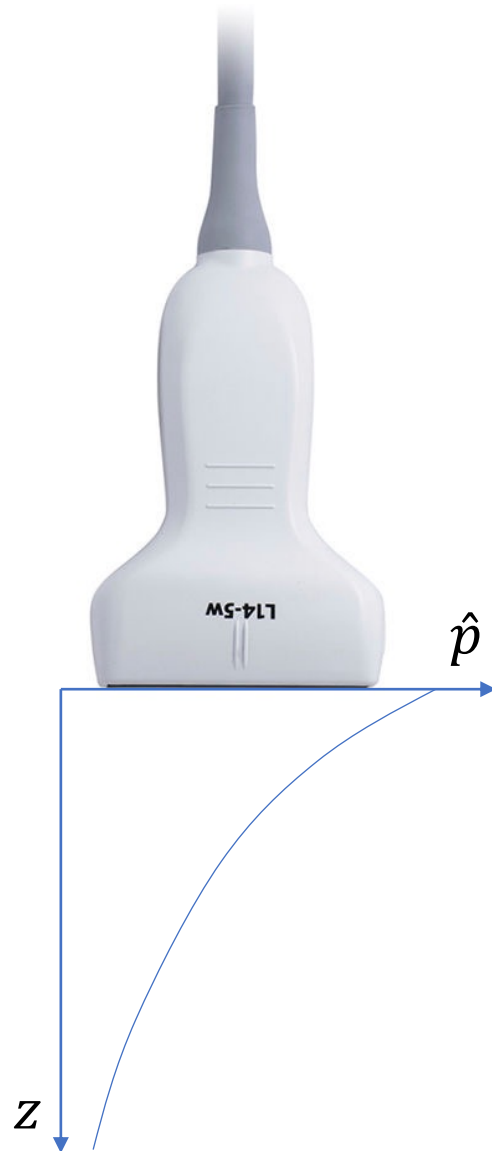
$$T_I = 1 - R^2$$



Ultrasound reflection coefficients in the body (ballpark)



Attenuation = absorption + scattering (planar wave)



$$\alpha = \alpha_{\text{abs}} + \alpha_{\text{scat}}$$

$$\hat{p}(z) = \hat{p}_{z=0} 10^{-\frac{\alpha_{\text{dB}} z}{20}}$$

$$\hat{p}(z) = \hat{p}_{z=0} e^{-\alpha_{\text{Np}} z}$$

α = attenuation coefficient

α_{abs} = absorption coefficient

α_{scat} = scattering coefficient

α_{dB} = attenuation coefficient in dB/cm

α_{Np} = attenuation coefficient in Neper/cm

p_0 = pressure at $z = 0$

p = peak pressure amplitude

z = distance

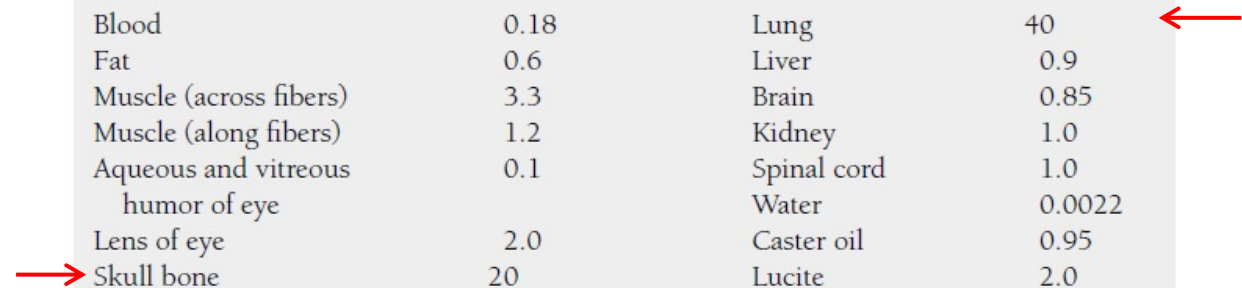
Attenuation

- In tissue sound energy is attenuated due to scattering and absorption

Tissue or Material	α (db/cm) @ f MHz	$\alpha = a \cdot f^b$	
		a [db/ (cm MHz)]	b
Water	—	0.002	2
Blood	—	0.15	1.21
Fat	—	0.6	1
Liver	—	0.9	1.1
Kidney	—	1	1
Brain	—	0.8	1.35
Heart	2 @1 MHz	—	—
Muscle (along the fibers)	1.3 @1 MHz	—	—
Muscle (across the fibers)	3.3 @1 MHz	—	—
Skin	9.2 @5 MHz	—	—
Eye (lens)	7.8 @10MHz	2	—
Eye (vitreous humor)	0.6 @6MHz	—	—
Bone (skull)	—	20	—
Bone (trabecular)	2–15 @ 0.2–1 MHz	—	—
Teeth (dentine)	80 @18MHz	—	—
Teeth (enamel)	120 @18MHz	—	—

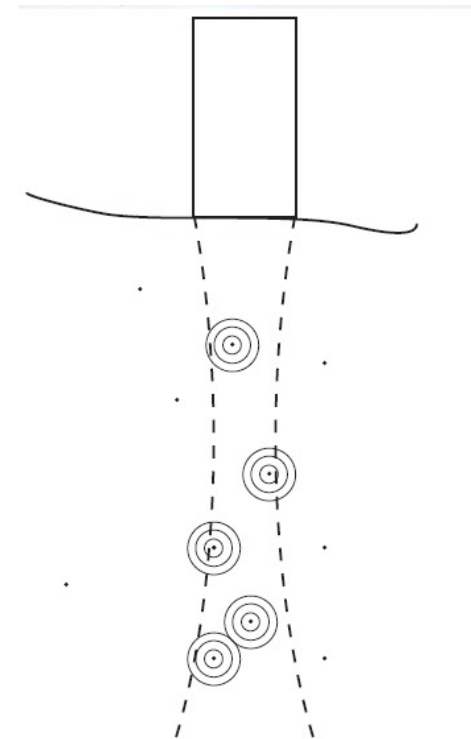
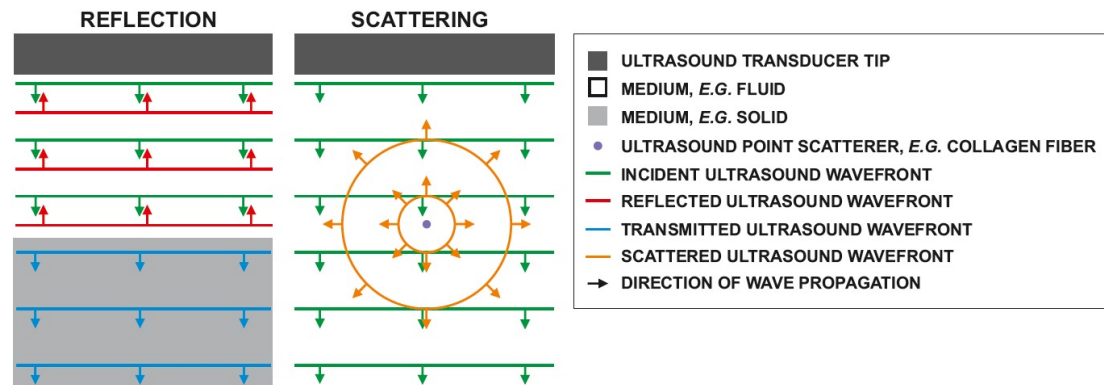
TABLE 19-4 Attenuation Coefficients α for 1-MHz Ultrasound

Material	α (dB/cm)	Material	α (dB/cm)
Blood	0.18	Lung	40
Fat	0.6	Liver	0.9
Muscle (across fibers)	3.3	Brain	0.85
Muscle (along fibers)	1.2	Kidney	1.0
Aqueous and vitreous humor of eye	0.1	Spinal cord	1.0
Lens of eye	2.0	Water	0.0022
Skull bone	20	Caster oil	0.95
		Lucite	2.0



Absorption & scattering

- Sound energy is eventually absorbed as heat
- Scattering occurs when the reflector size is close to that of wavelength



Geometric attenuation

- Planar source: $p_2 = p_1 e^{-\alpha x}$

$$I_2 = I_1 e^{-2\alpha x}$$

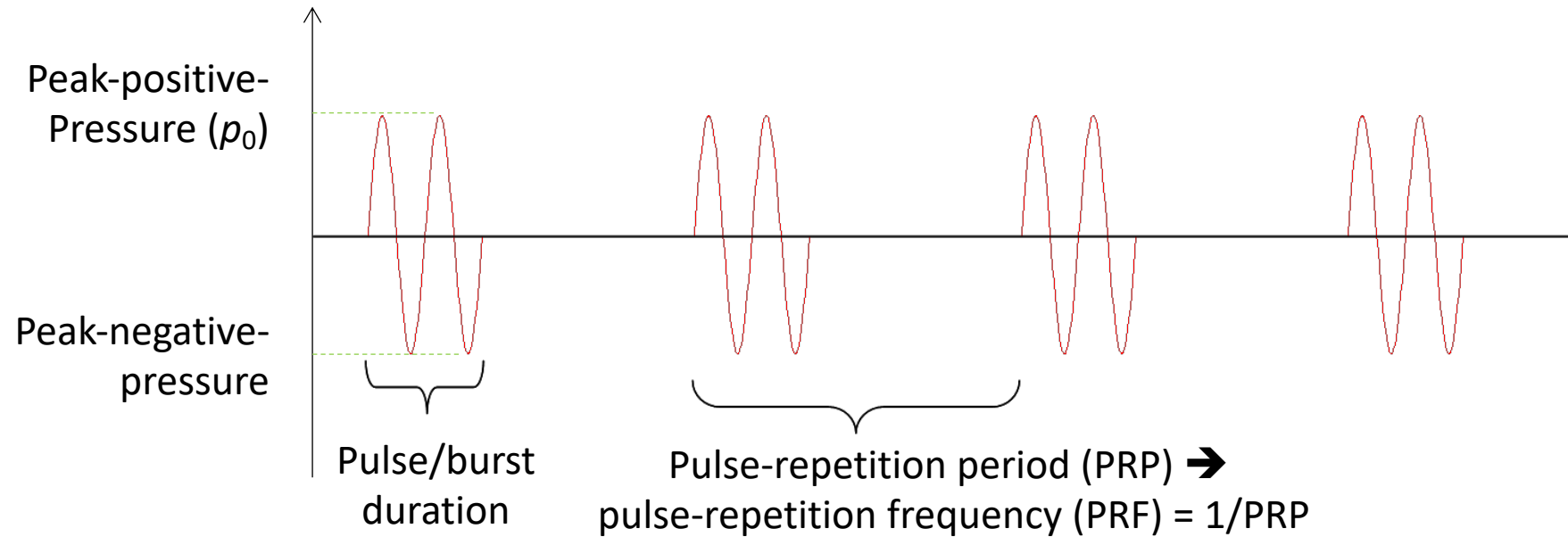
$$\alpha = -\frac{1}{2x} \ln \frac{I_2}{I_1} = \frac{1}{2x} \ln \frac{I_1}{I_2} \quad \text{Unit: Np/cm}$$

- Line source: $I_2 = ? I_1 e^{-2\alpha r}$ $p_2 = ? p_1 e^{-\alpha r}$

- Point source: $I_2 = ? I_1 e^{-2\alpha r}$ $p_2 = ? p_1 e^{-\alpha r}$

} Exercises

Pulse/burst concepts

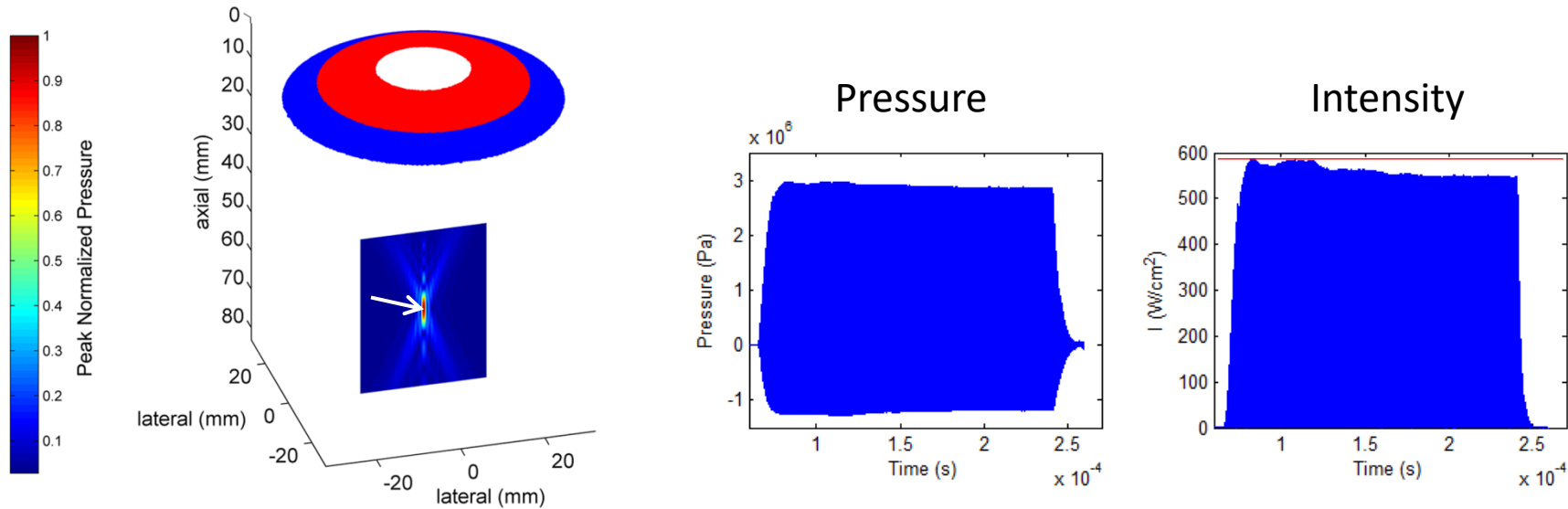


Duty cycle = the % of time when ultrasound is **ON** (in this example duty cycle is about 40%)

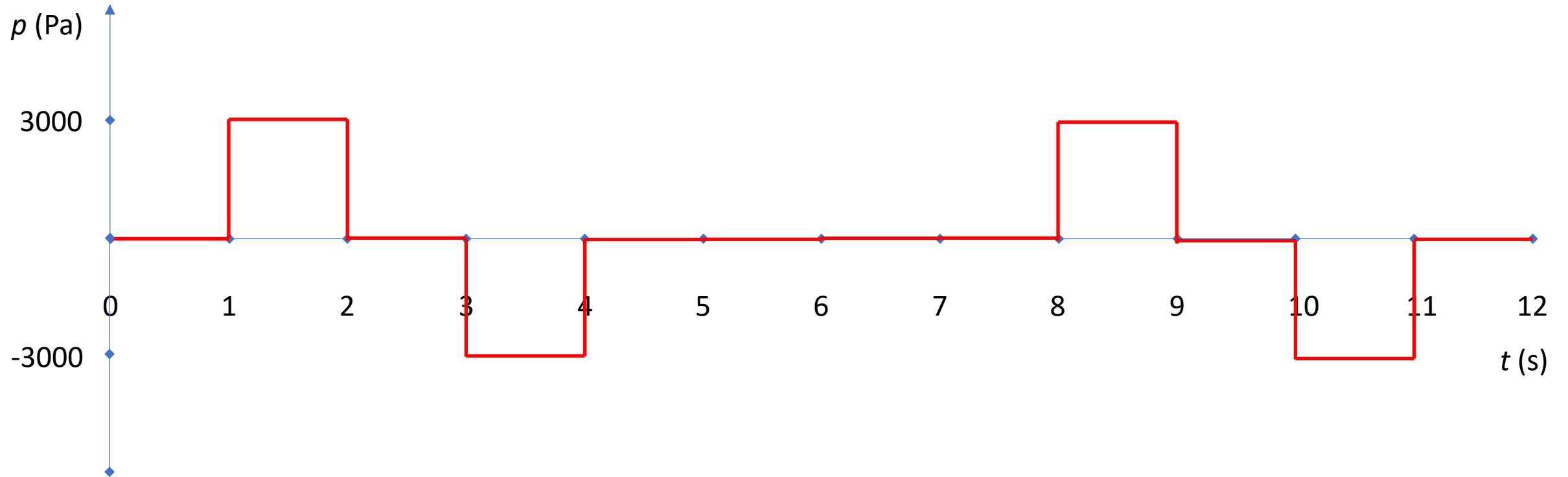
I_{sptp}

- **Spatial peak temporal peak intensity (unit:W/m or more commonly W/cm²)**
 - Intensity of the spatiotemporally the hottest "spot" in the field

$$I_{\text{sptp}} = \{I(t, x, y, z)\}_{\text{max}} = \left\{ \frac{p^2(t, x, y, z)}{\rho c} \right\}_{\text{max}}$$

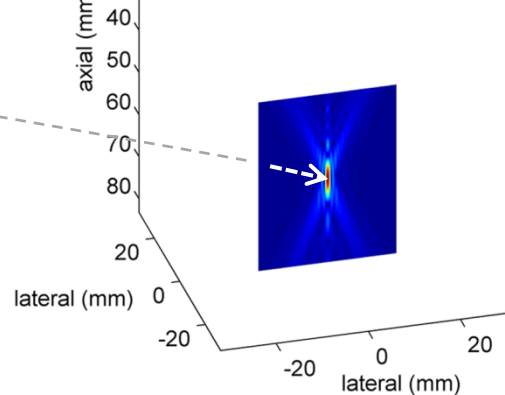
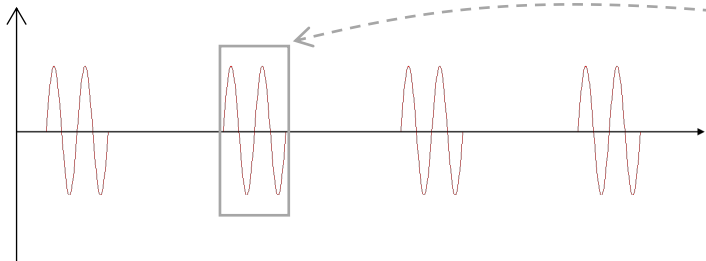


What is T , f , PRP, PRF, and I_{sptp} ?



Assume that the signal is from the location of spatial peak and the wave propagates in water.

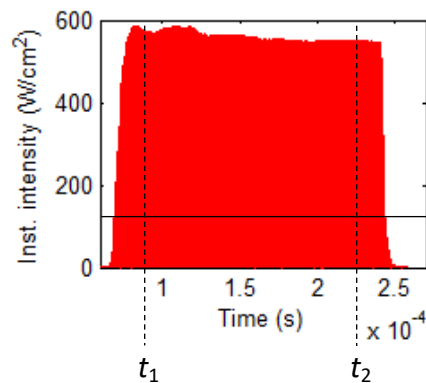
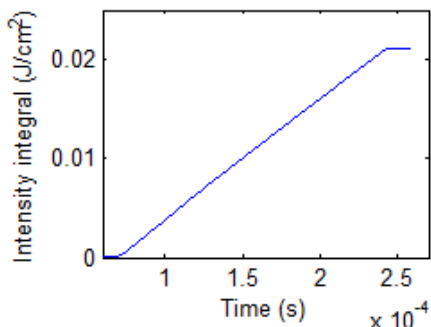
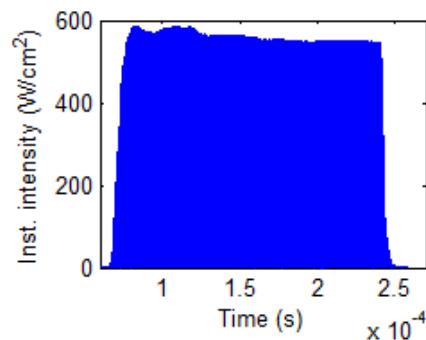
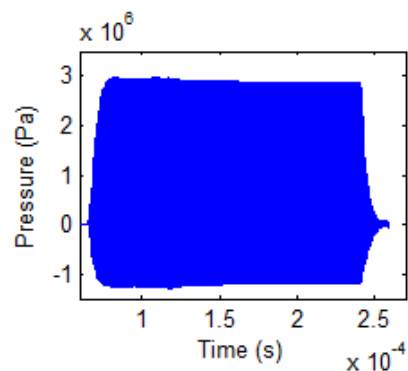
I_{sppa}



- **Spatial peak pulse average intensity**

- Describes power of at the focus per unit area during a single pulse/burst at the hottest spot

$$I_{\text{sppa}} = \frac{\int p^2(t) dt}{\rho c PD}$$



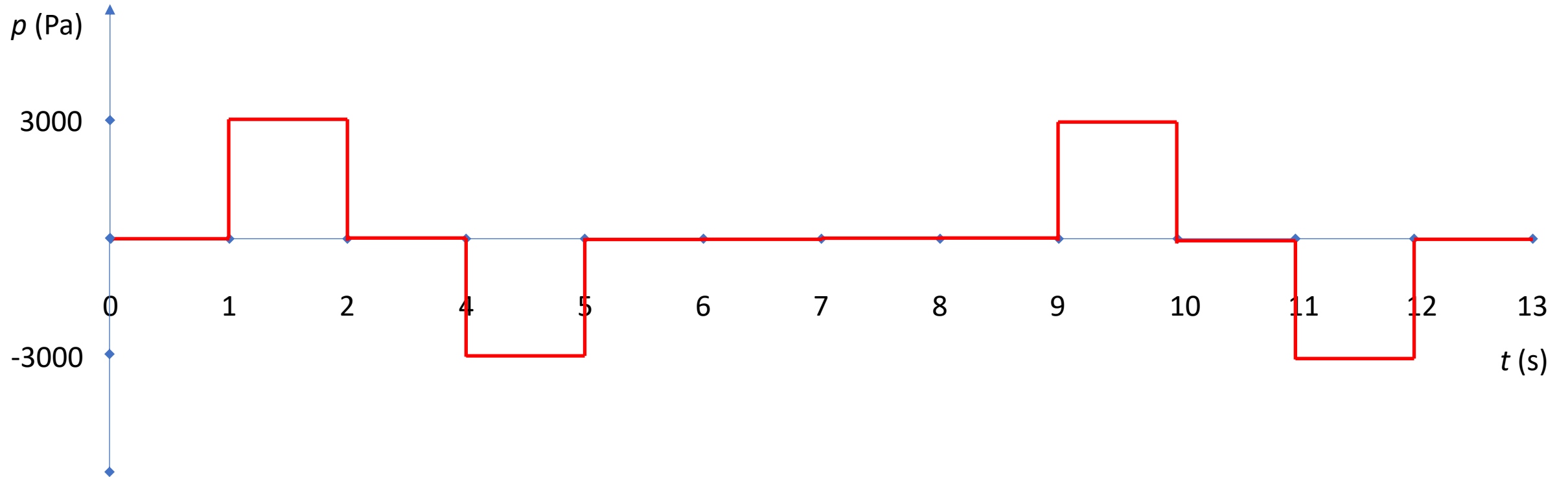
PD is defined as the 1.25 x the interval between time points, where intensity integral reaches 10% (t_1) and 90% (t_2) of the maximum.

Integration is conducted over the entire pulse/burst.

$$PD = 138 \mu\text{s}$$

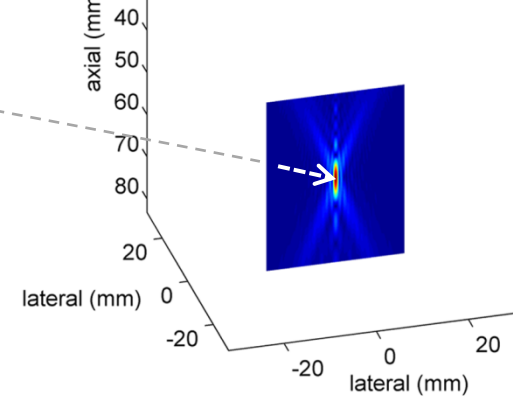
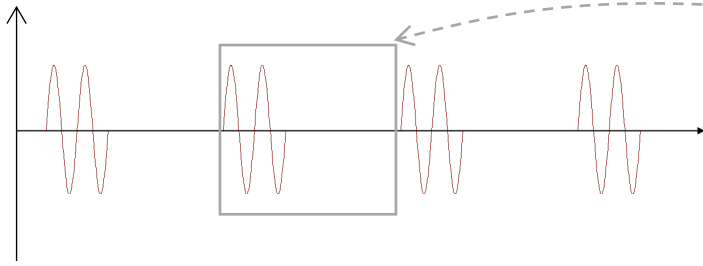
$$I_{\text{sppa}} = 123 \text{ W/cm}^2$$

What is PD and I_{sppa} ?



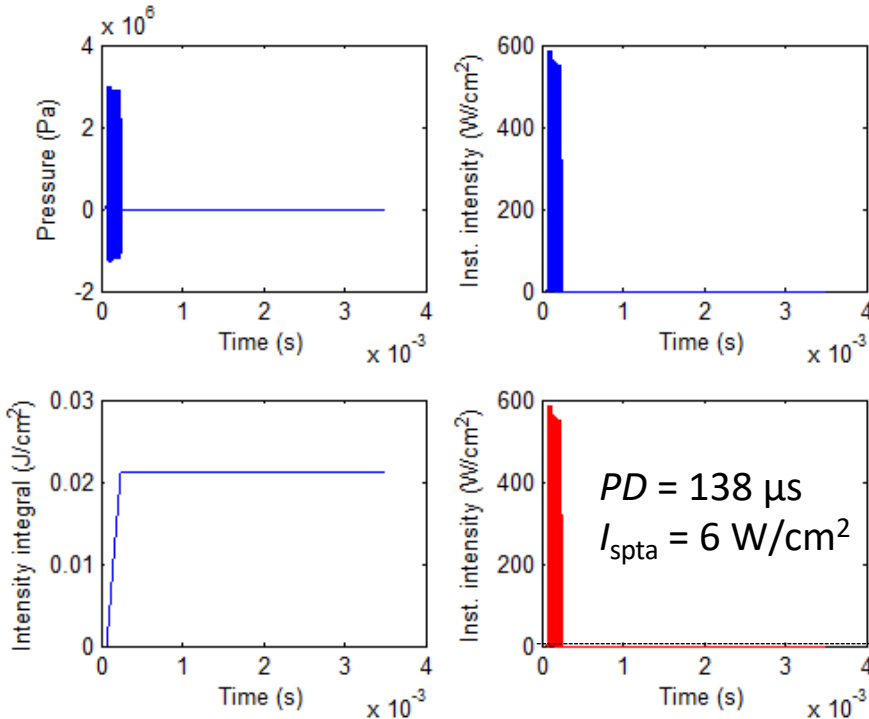
Assume that the signal is from the location of spatial peak.

I_{spta}



- **Spatial peak time average intensity**

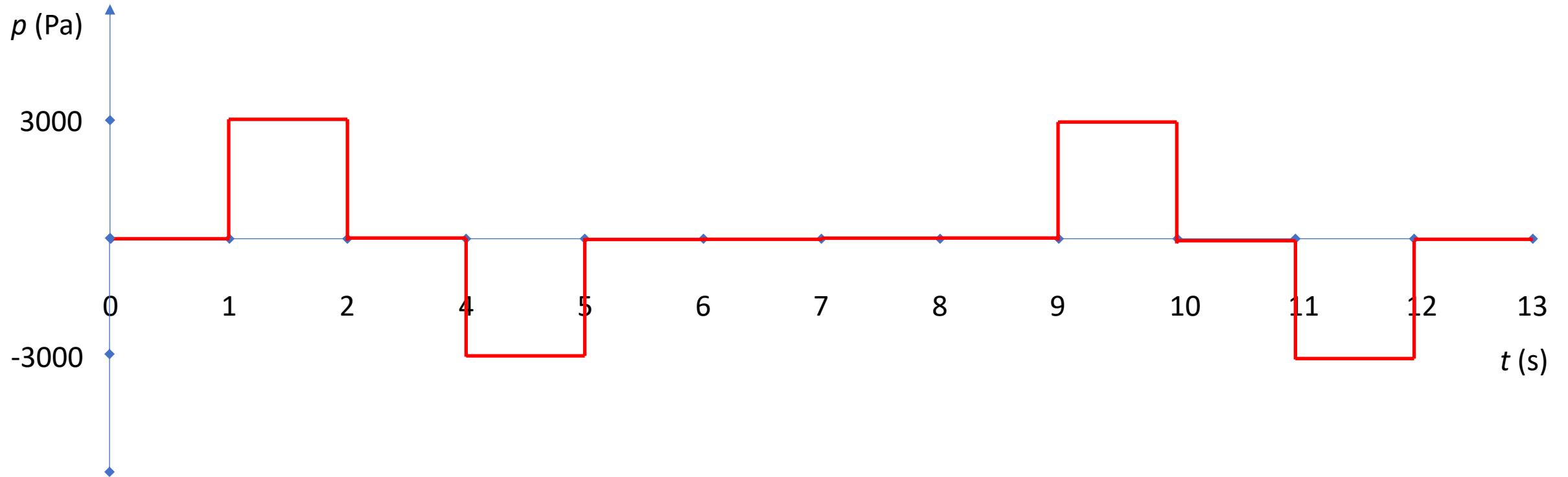
- Describes the average power at focus across unit area during one PRP at the hottest spot



$$I_{sppa} = \frac{\int_{t_1}^{t_2} p^2(t) dt}{\rho c PRP}$$

PRP = pulse repetition period
= $t_2 - t_1$ = time from the beginning of a pulse/burst to the beginning of the next pulse

What is PRP and I_{spta} ?



Assume that the signal is from the location of spatial peak.

Feedback on this session

<https://presemo.aalto.fi/bmusquiz>

