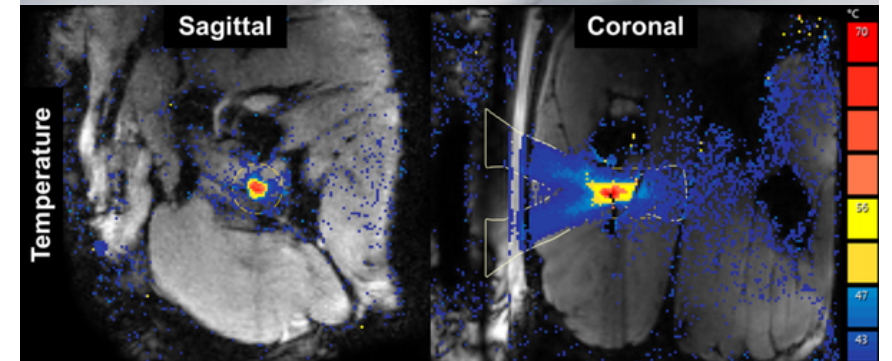
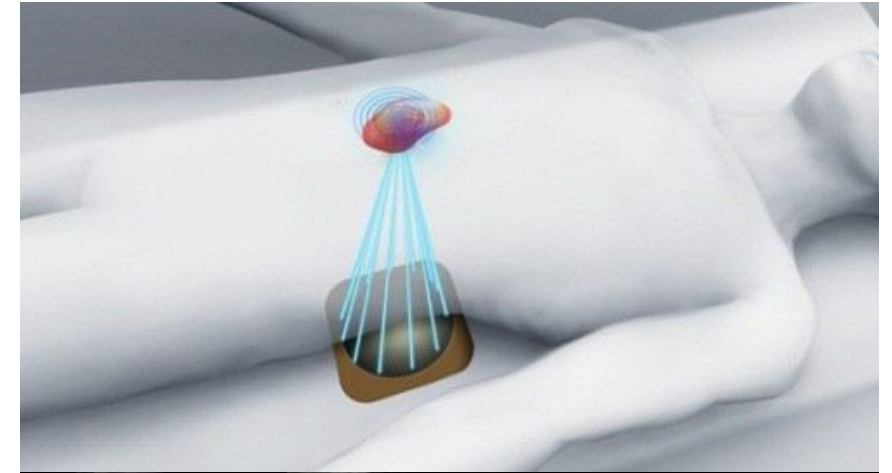
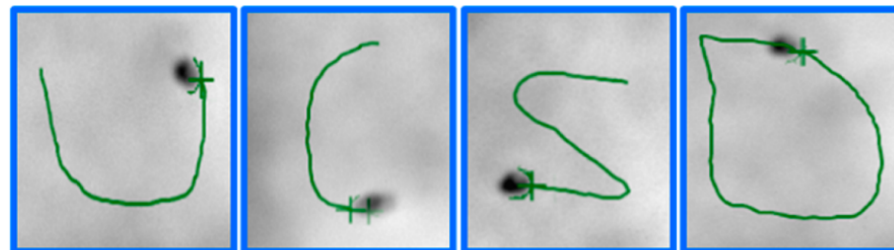
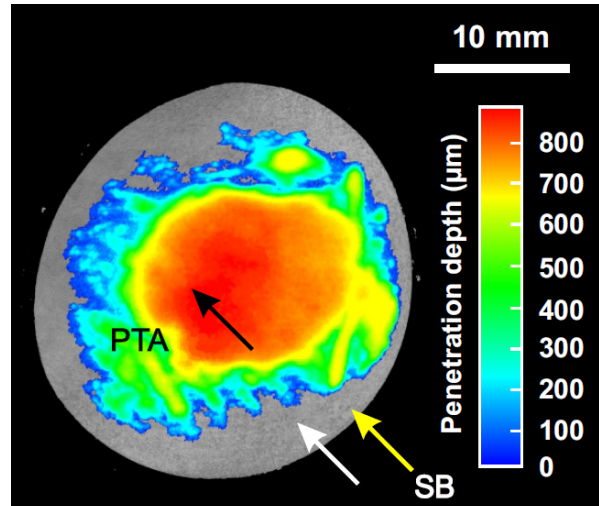


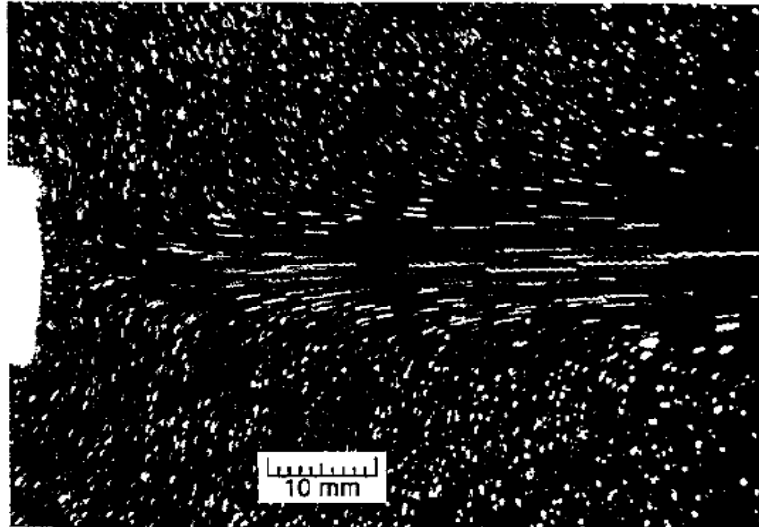
# Biomedical Ultrasonics, 5 cr

Heikki Nieminen

7.1.-31.5.2019

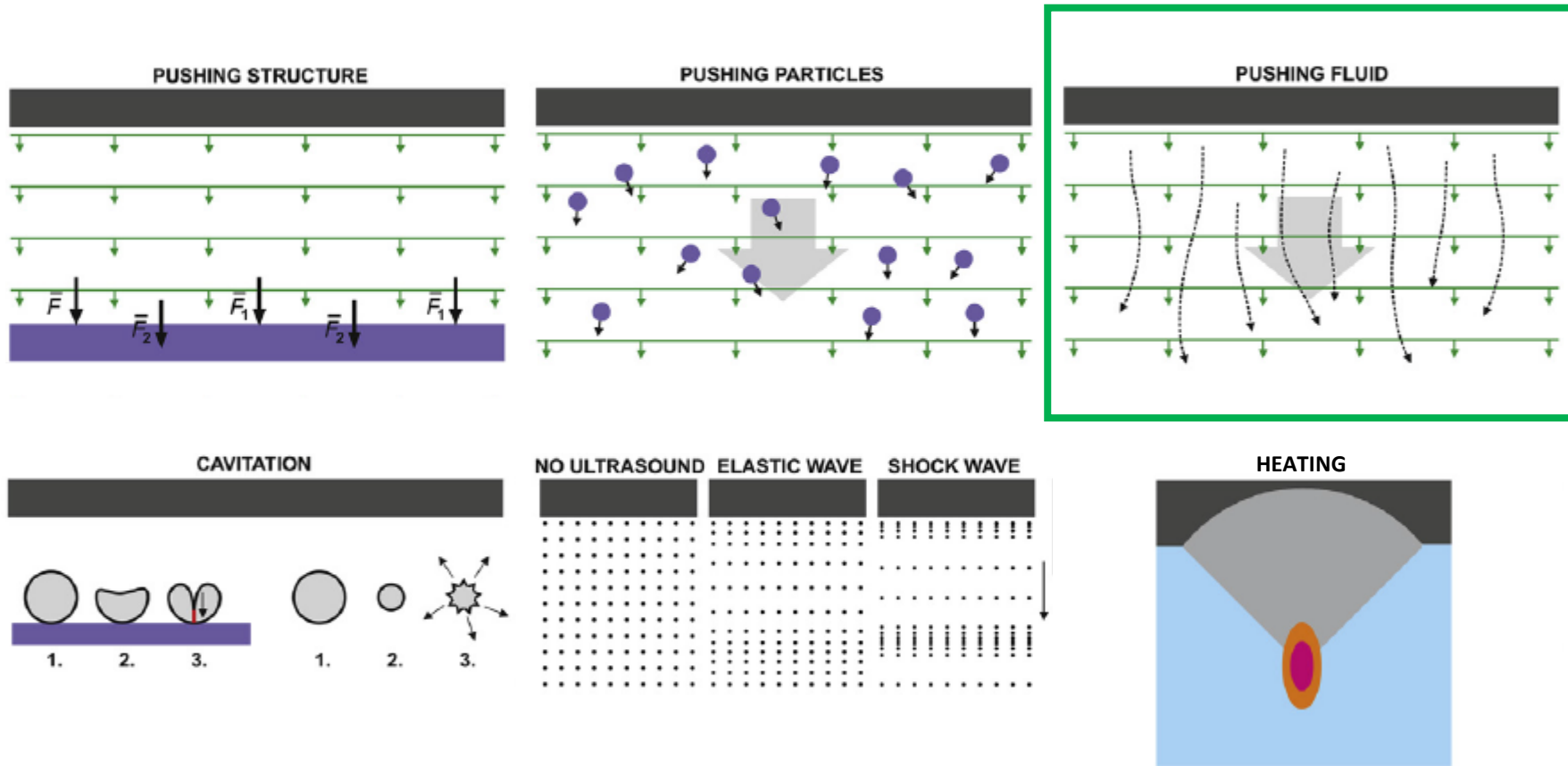


# Acoustic streaming



Duck et al 1998.

# Non-linear ultrasonics



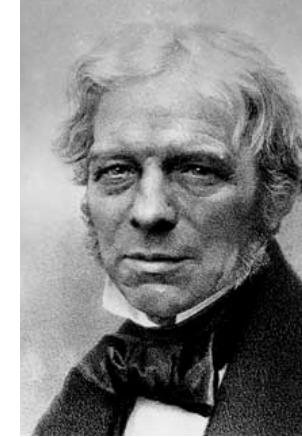
# Questions

- What is needed to generate radiation force in tissue?
- What actually happens in the tissue when a constant radiation force is applied?
- What happens when the radiation force is applied on a fluid volume?

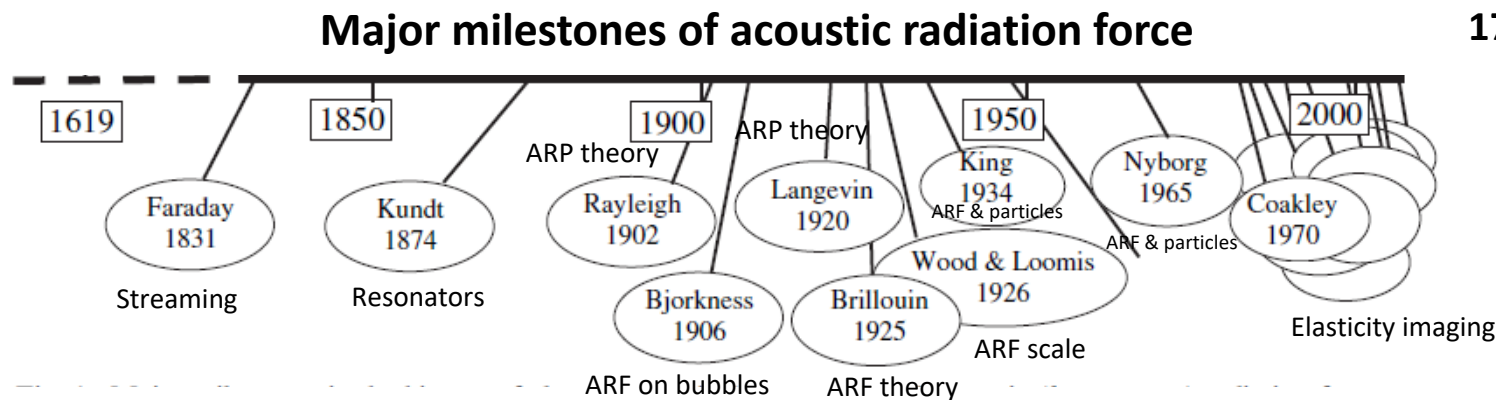


# Acoustic streaming

- Acoustic streaming was originally discovered by Faraday in 1831
- Faraday observed that very light powder moved near a sound source



**Michael Faraday**  
1791-1867



## Reading:

Sarvazyan et al. 2010: <http://www.sciencedirect.com/science/article/pii/S0301562910002450> (not accessible inside Uni. Helsinki)

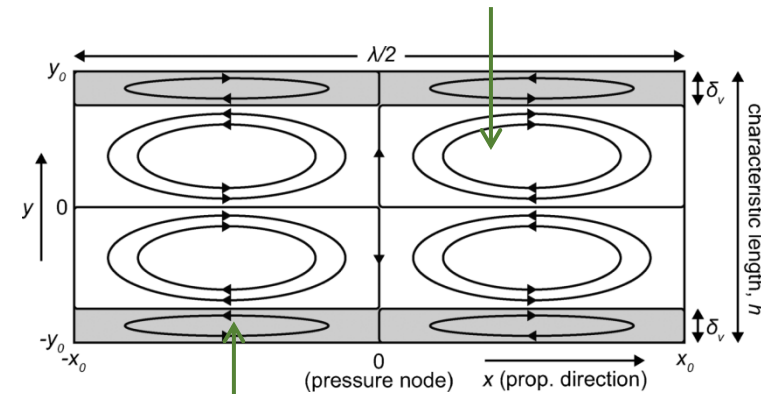
# Acoustic streaming

- In the following, we deal with three forms of acoustic streaming:
  - Eckart streaming
  - Rayleigh streaming
  - Schlichting streaming

**Eckart streaming**



**Rayleigh streaming**



**Schlichting streaming**

# Different forms of acoustic streaming

## CLASSIC TERMS FOR ACOUSTIC STREAMING

Eckart streaming is acoustic streaming within the fluid bulk, away from the sound source (Eckart 1948). It appears over length scales greater than one sound wavelength in the fluid, due to viscous attenuation of the sound radiating into the fluid from the source. If the fluid size is less than one wavelength, this streaming may not appear.

Rayleigh streaming is acoustic streaming in the bulk of a fluid typically in a vortical pattern, with each vortex having a scale of one wavelength in the fluid (Rayleigh 1884). It appears because of streaming present in the viscous boundary layer surrounding the fluid bulk.

Schlichting streaming is acoustic streaming within the viscous boundary layer toward the source of acoustic energy due to viscous attenuation (Schlichting 1932). Because the viscous boundary layer is typically much smaller than the acoustic wavelength, this streaming is the most fine-grained of the three.

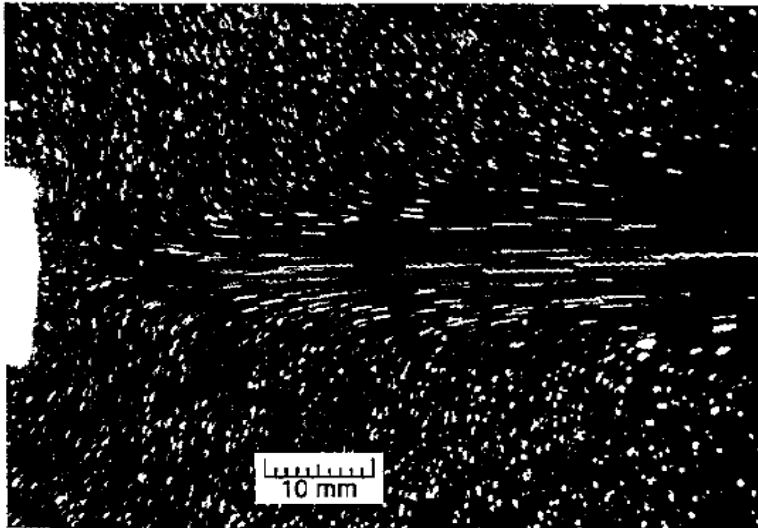
All these streaming terms are used in the literature as extensions of the forms of streaming reported by the respective authors, and not always correctly. The important aspects to keep in mind are the dominance of one form of streaming over another, depending on the scale of the fluid system, and the potential to have all three forms of streaming, giving rise to very complex phenomena.

# Acoustic radiation force in fluids = **acoustic streaming**

- *Acoustic streaming a.k.a quartz wind*
- Radiation force in absorbing medium (**solid or fluid**):  $F_{abs} = 2\alpha I_{ta} / c$   
Unit: N/m<sup>3</sup> or Pa/m      Unit for  $\alpha$ : Np/m
- The interpretation of this equation is that it actually is the *force exerted per volume unit or Pascals per length unit*
- By applying radiation force on absorbing fluid one can generate flow of fluid that is generated along the axis of sound propagation

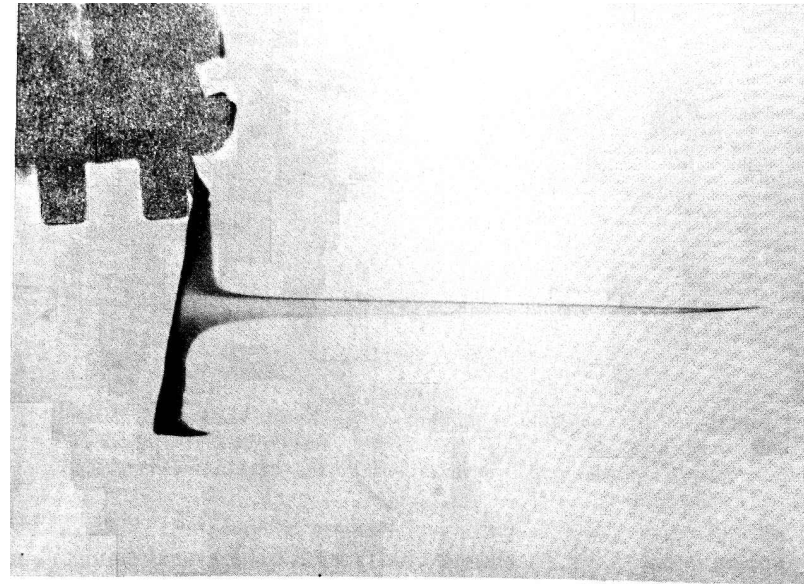
# Acoustic streaming

## Particle transport



**Figure 3.2.** Photograph of streaming motion induced in water by a weakly focused 1 MHz transducer. The radiation pressure field is shown in figure 3.1. Exposure time 1 s.

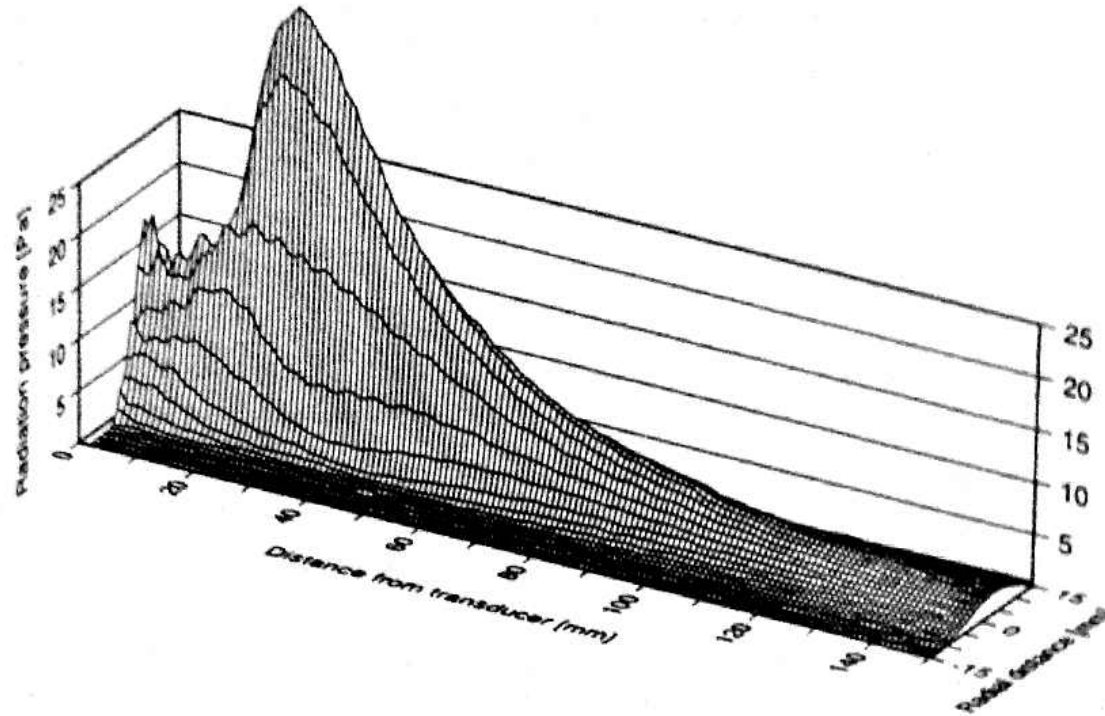
## Contrast agent transport



**Figure 3.5.** Acoustic streaming demonstrated using thymol blue for a 3 MHz pulsed beam. (From Starritt et al (1991), with permission.)

# Radiation pressure example

- Describe how the axial and radial radiation pressures affect streaming:



**Figure 3.1.** Measured radiation pressure field from a weakly focused 1 MHz transducer. (From Hertz (1993) with permission.)

# Acoustic streaming video



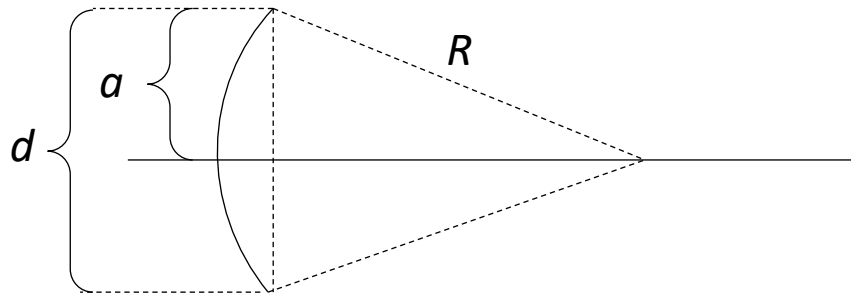
<http://www.youtube.com/embed/ArpclLD4yP8>

# Streaming velocity

- Streaming velocity  $v$  in the focus of a focused beam can be approximated as follows:

$$v = \left( \frac{2\alpha I_{\text{ta}}}{c\nu} \right) d^2 G$$

$\nu = \eta/\rho =$  kinematic viscosity  
 $\eta =$  shear viscosity



$G = \frac{\pi a^2}{\lambda R}$  is the geometric factor

Weak focus:  $0 < G \leq 2$

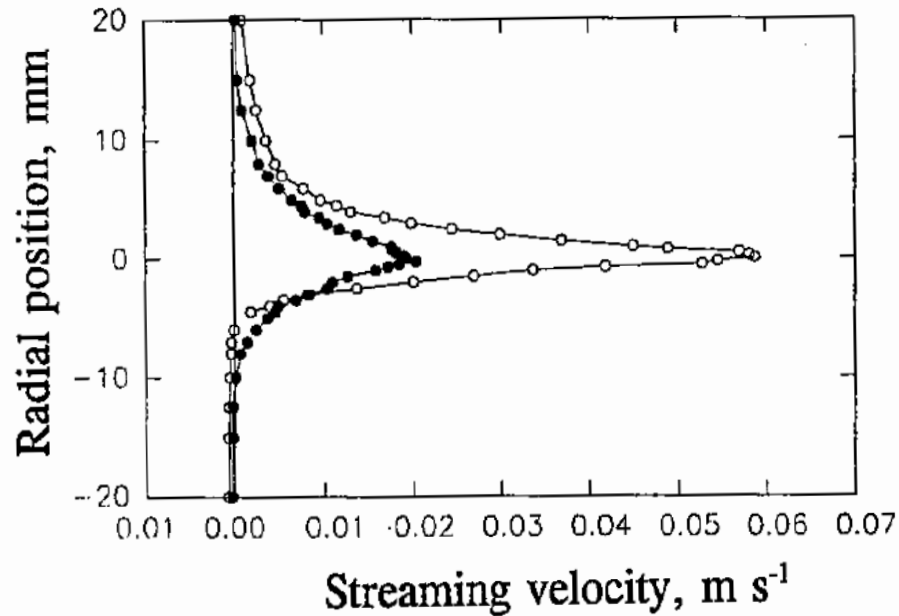
Medium focus:  $2 < G \leq 2\pi$

Strong focus  $G < 2\pi$

- This streaming, *i.e.* Eckart streaming, is different to Rayleigh streaming, because there is net mass transfer
- Any absorption mechanism can contribute to the absorption term " $\alpha$ " (shear viscosity, kinematic viscosity, "excess absorption due to non-linearity etc.")



# CW LIUS vs. shocked pulsed beam

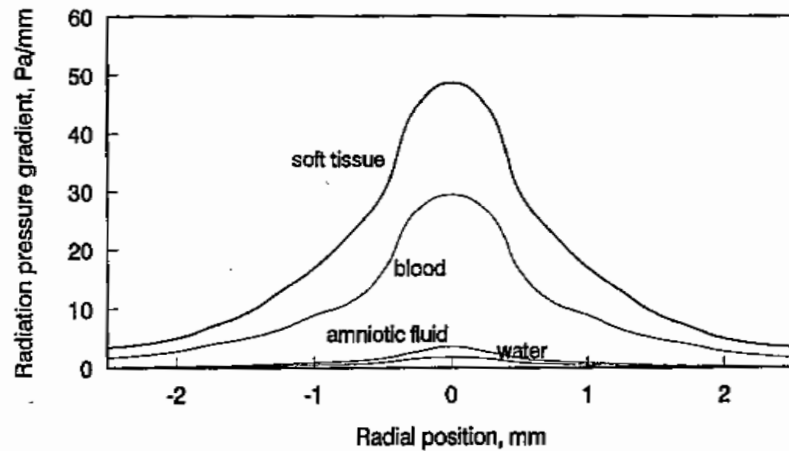


The average intensities are the same

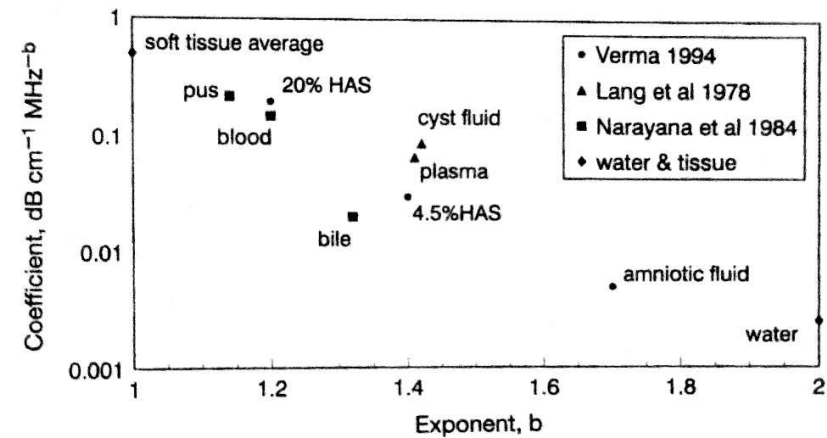
Why do the streaming profiles differ?

*Total acoustic power was 150 mW in both cases. ● continuous wave, low amplitude beam; ○ strongly shocked pulsed beam, 1.4 μs pulse length, 10.1 kHz prf, 1.20 W cm<sup>-2</sup> time-average intensity. The beam width at the focus was 2.5 mm.*

# Radiation pressure gradient in different tissues/media



**Figure 3.3.** Radial profiles of radiation pressure gradients calculated from measured pulse intensities at the focus of a shocked, weakly focused beam in water. Frequency 3 MHz; pulse-average intensity  $118 \text{ W cm}^{-2}$ .



**Figure 3.4.** Attenuation coefficient,  $\alpha$ , for several biological liquids, expressed as  $\alpha = af^b$  in  $\text{dB cm}^{-1} \text{ MHz}^{-b}$ . The graph demonstrates the decrease of exponent from 2 (for water) to 1 (for soft tissue) as the attenuation at 1 MHz increases.

Note the effect of attenuation coefficient, beam profile and the radiation pressure

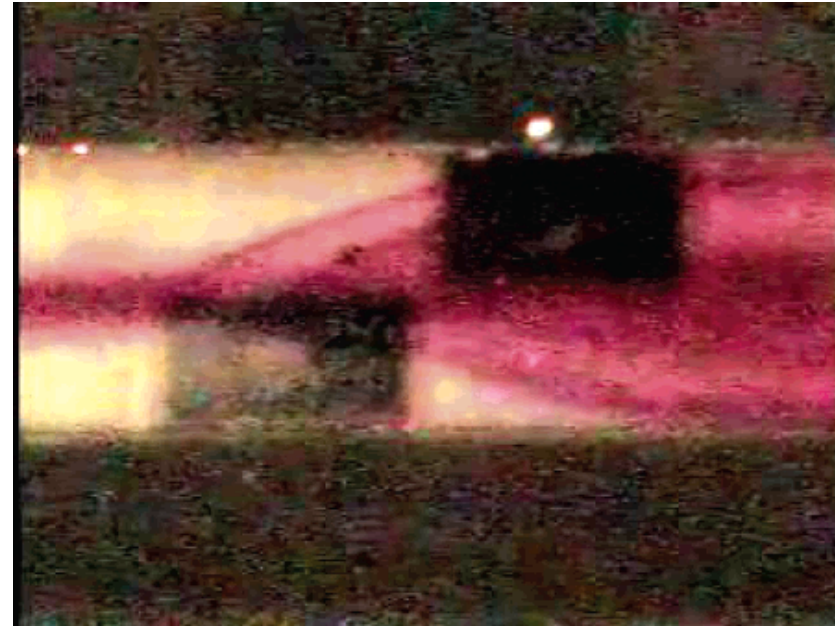
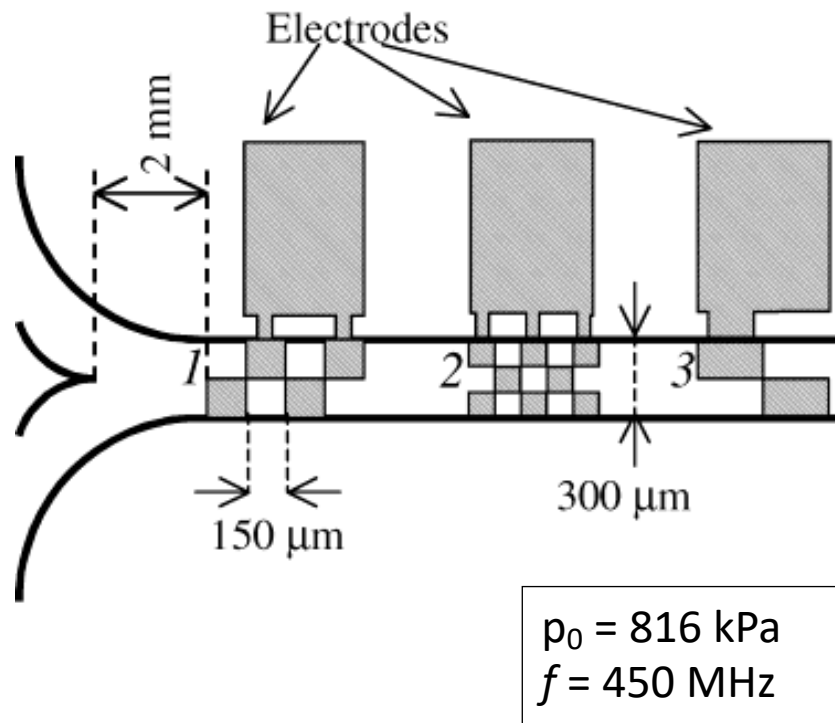
# Acoustic streaming *in vivo*

- Acoustic streaming is relatively commonly observed in the clinical context during imaging, but poorly documented
- Examples of streaming *in vivo*:
  - Cyst fluid in breast, ovary and testicle
  - Ventricular hemorrhage
  - Liquified vitreous humour

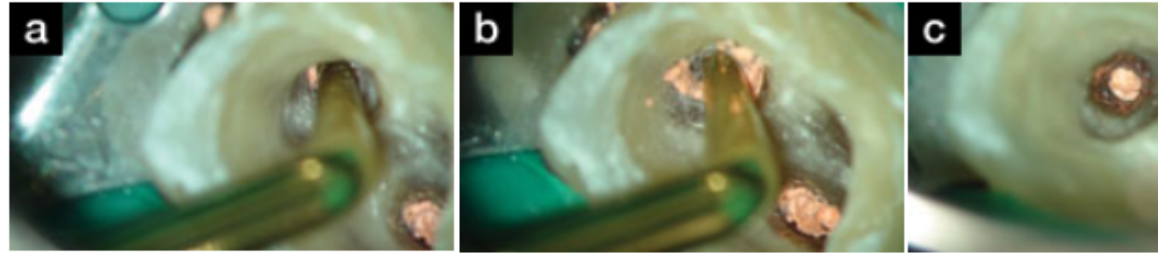
# Acoustic streaming examples

# Ultrasound-induced streaming turbulence

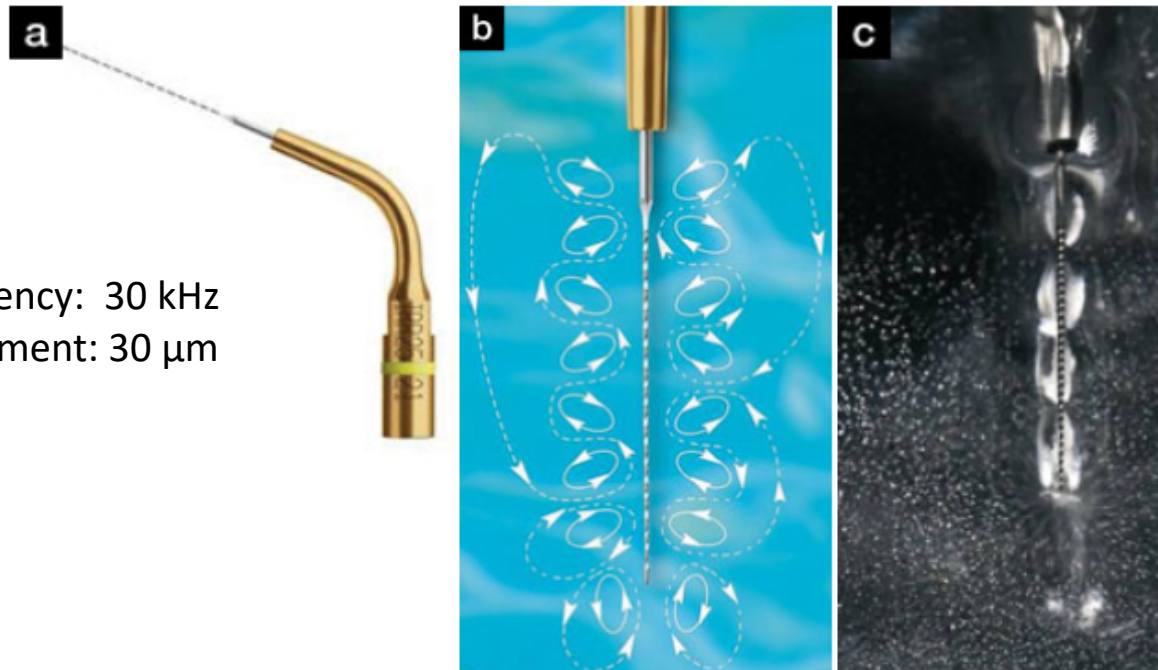
- Acoustic streaming
- Micro-fluidic mixer



# Dental irrigation

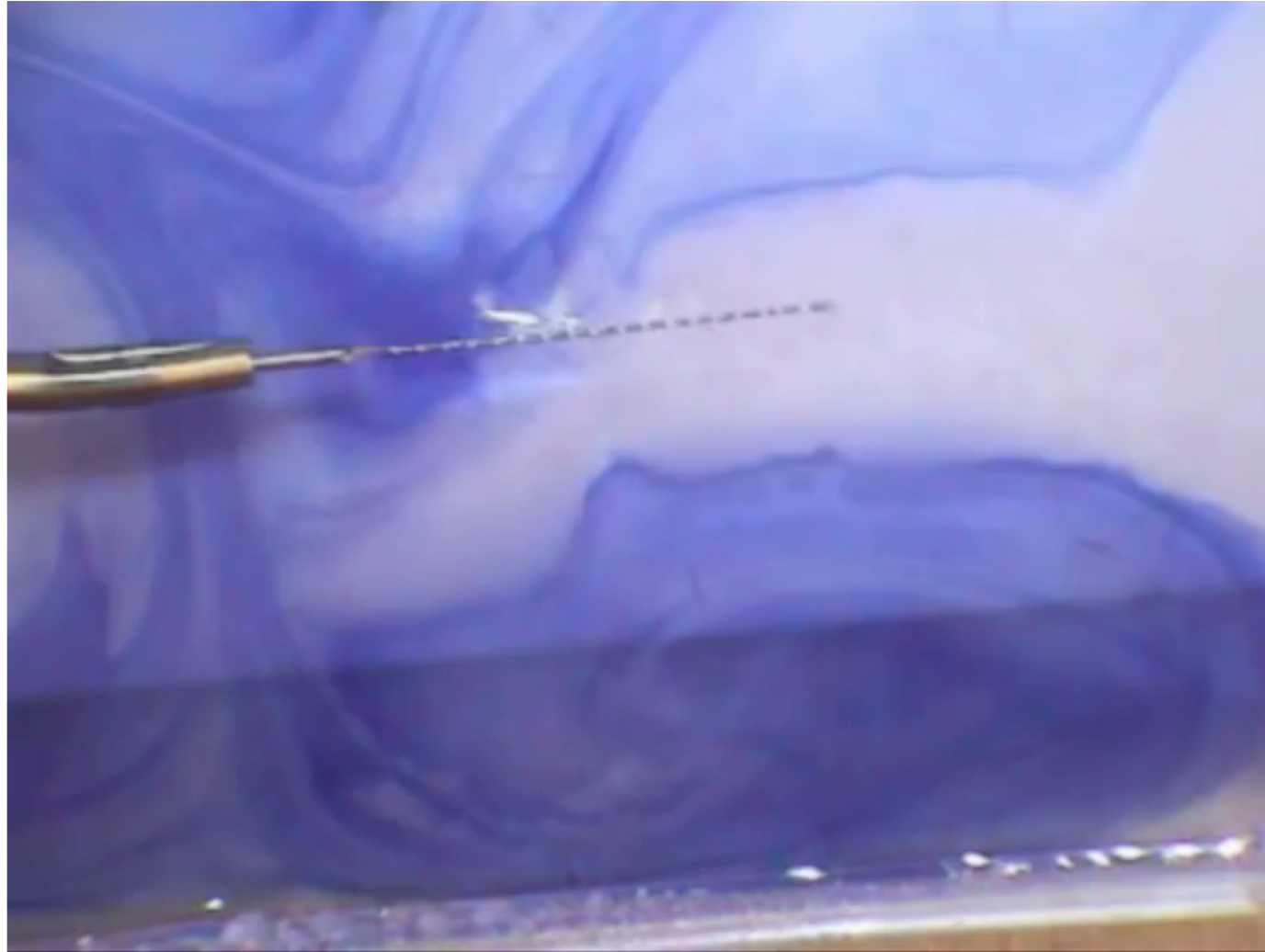


Figures 13a to 13c. BL-5 tips used deeper in the canal. (Courtesy of Dr. Yoshi Terauchi, Japan)



Operating frequency: 30 kHz  
Surface displacement: 30  $\mu$ m

# Acteon IrriSafe



<https://www.youtube.com/watch?v=3jaTPpEthTs>

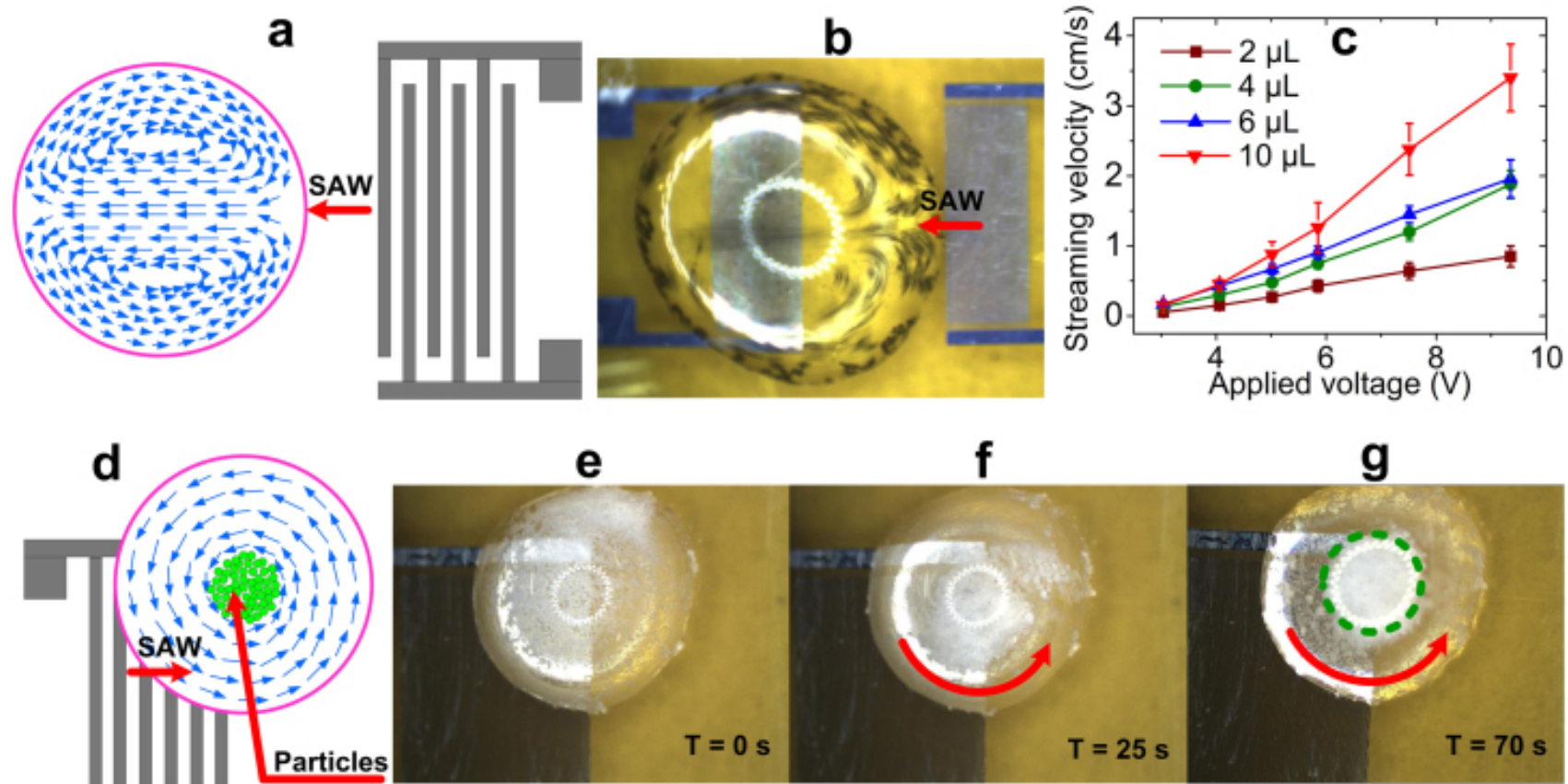
Acoustic streaming (SAW)



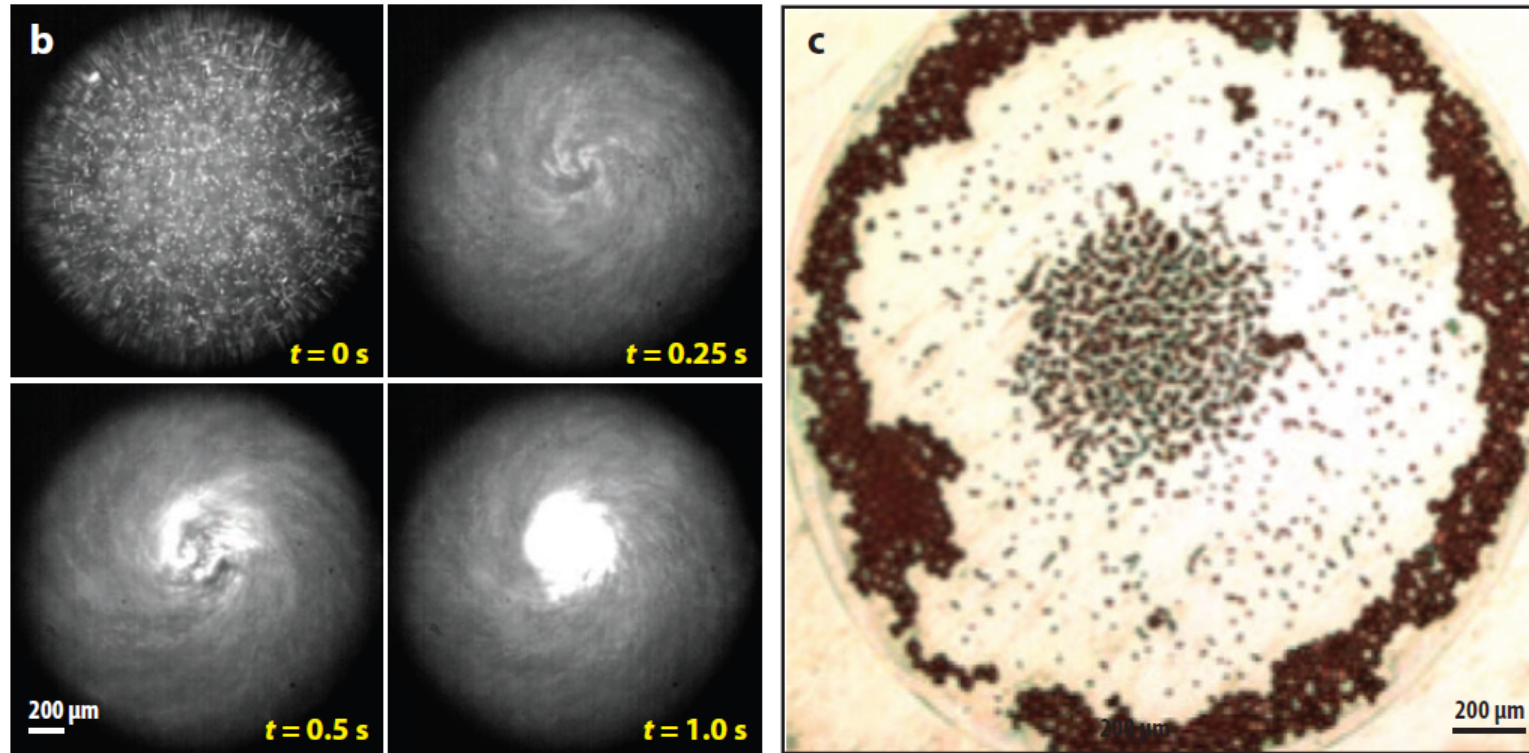
# Micro-centrifuging by breaking the symmetry



# Micro-centrifuging in small droplet



# Micro-centrifuging in micro-droplet



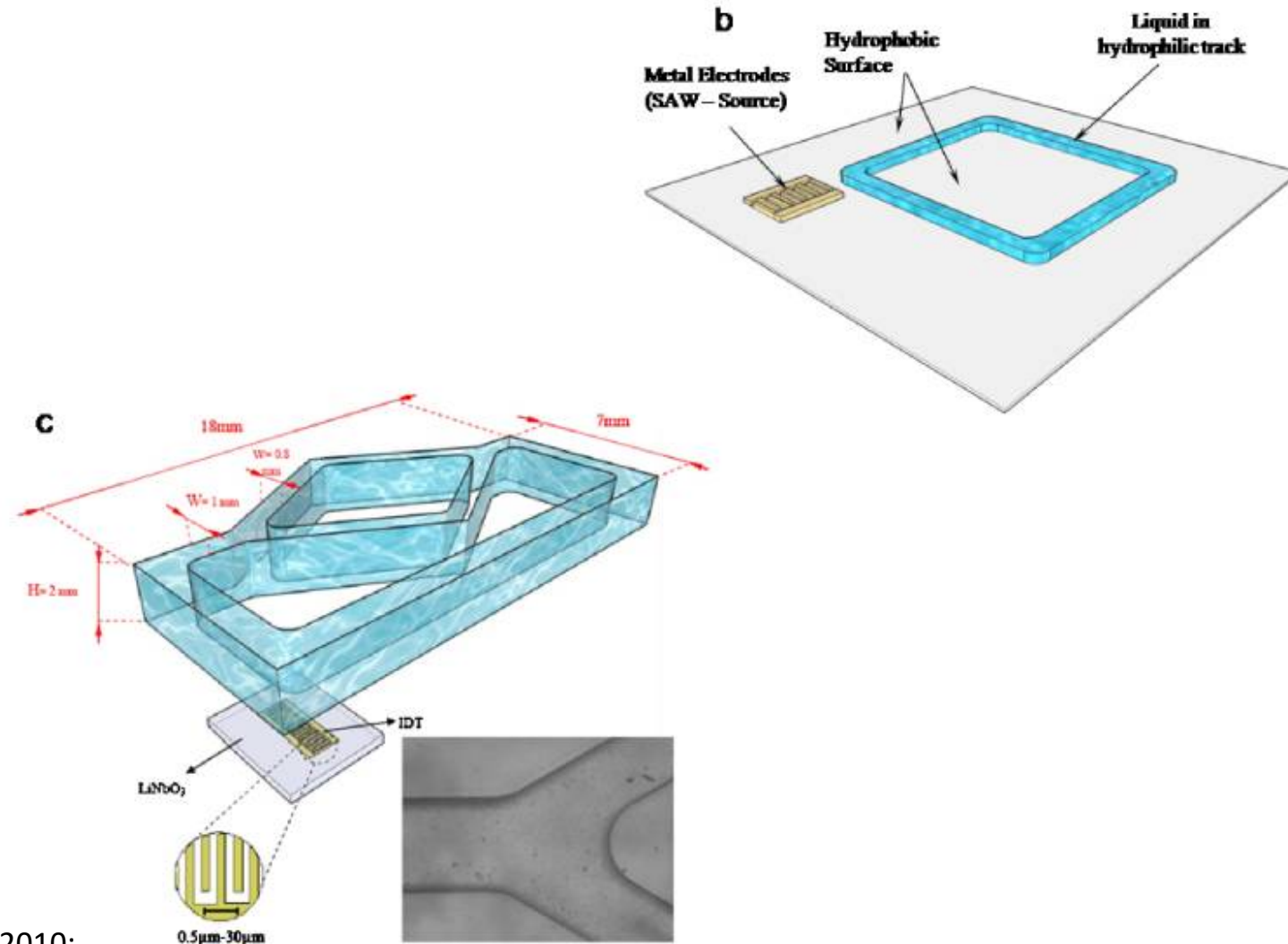
**Note the very short time scale!**

Leslie et al 2013:

<http://www.annualreviews.org/doi/pdf/10.1146/annurev-fluid-010313-141418>

How could this be used for drive-in?

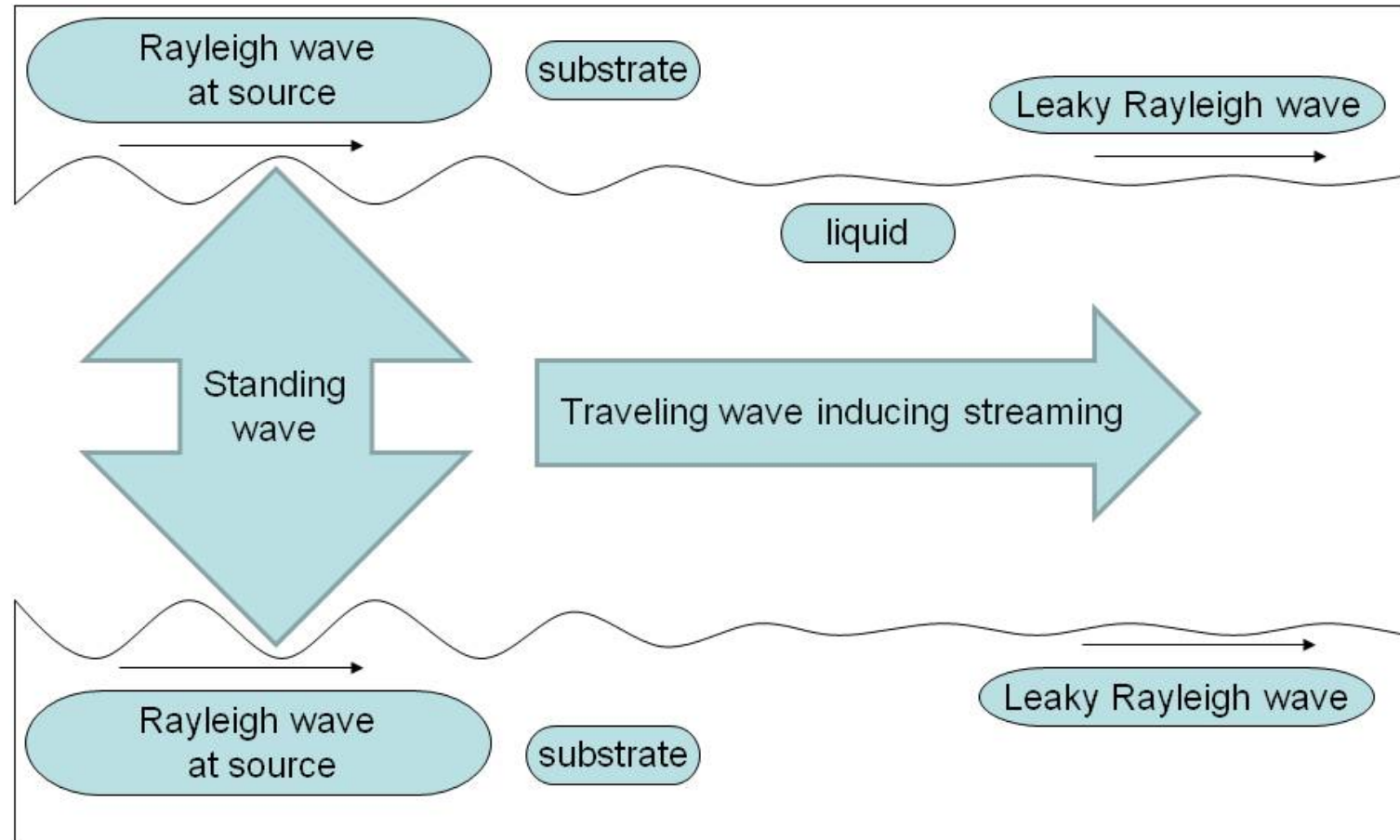
# Functionalized micro-fluidic channel to study cell adhesion



Fallah et al. 2010:

<http://www.ncbi.nlm.nih.gov/pmc/articles/PMC2917880/>

# Micro-pump





# SAW mixer

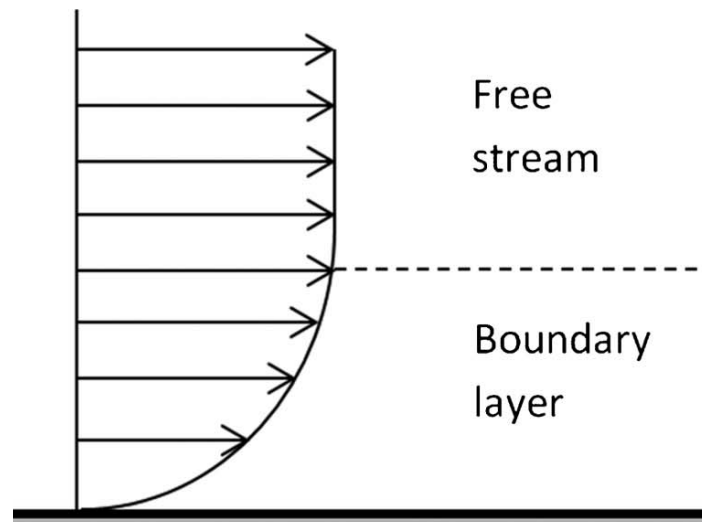


**Fig. 14** Surface acoustic wave (SAW) induced mixing in one well in a 96-well plate. The well diameter is approx. 6 mm. Figure taken from Wixforth.<sup>73</sup>

# Rayleigh and Schlichting streaming

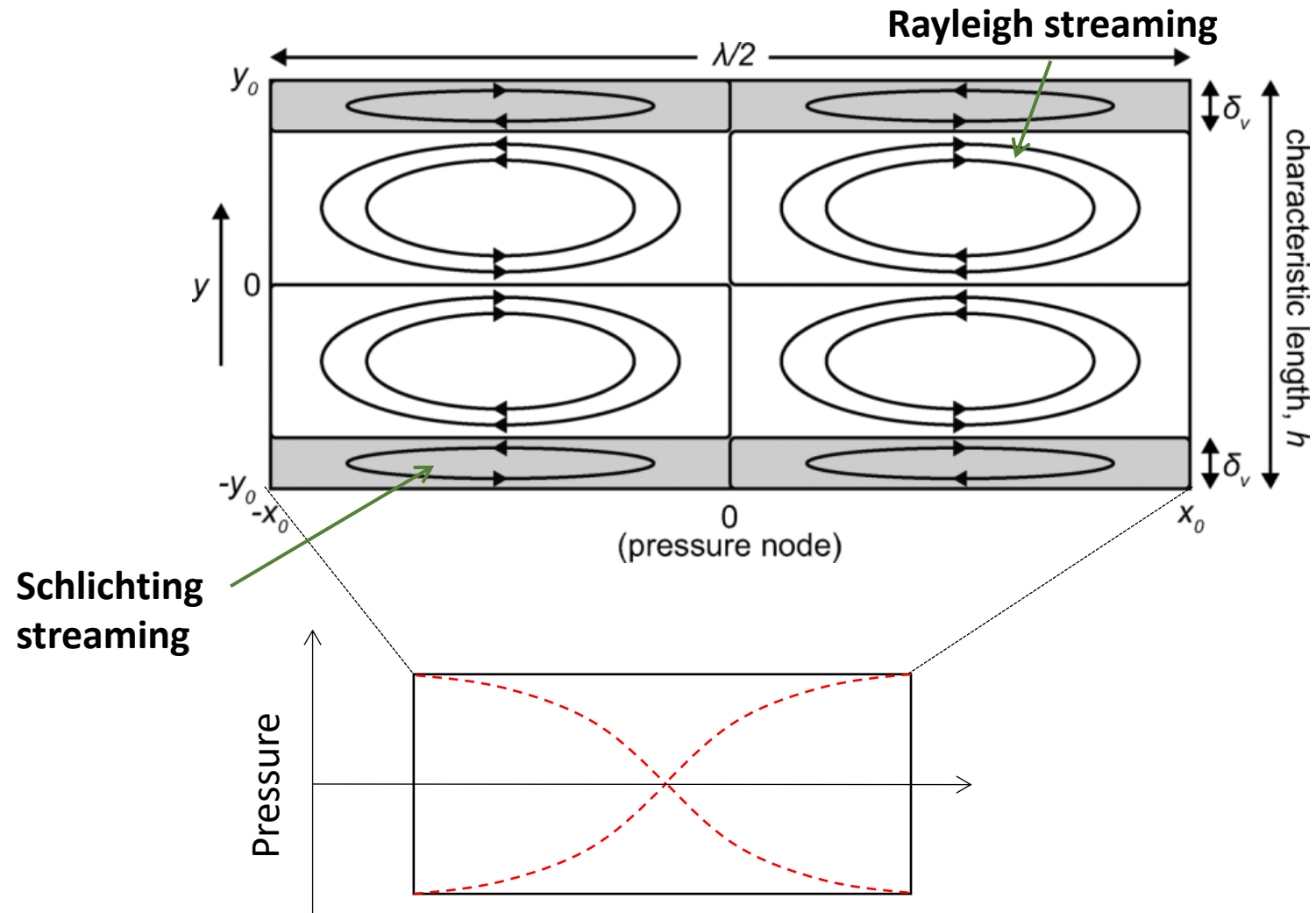
# Schlichting streaming

- We have learned that absorption of sound energy is converted to streaming
- Dissipation is amplified at boundaries due to viscosity
- Boundary layer:

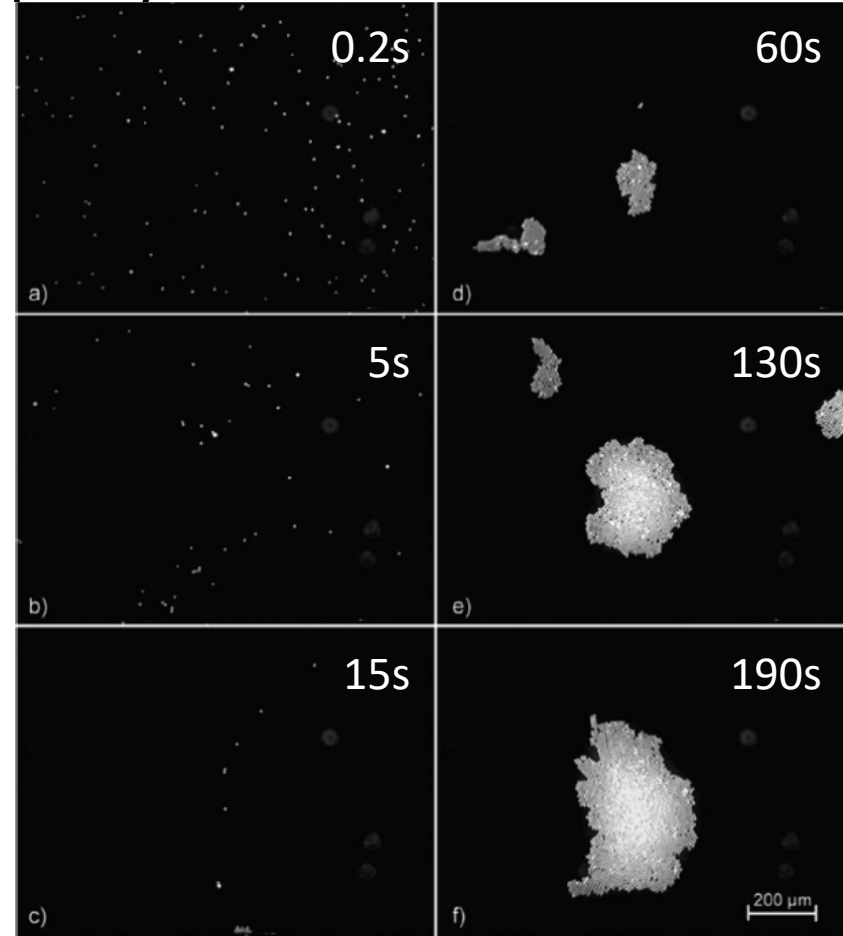
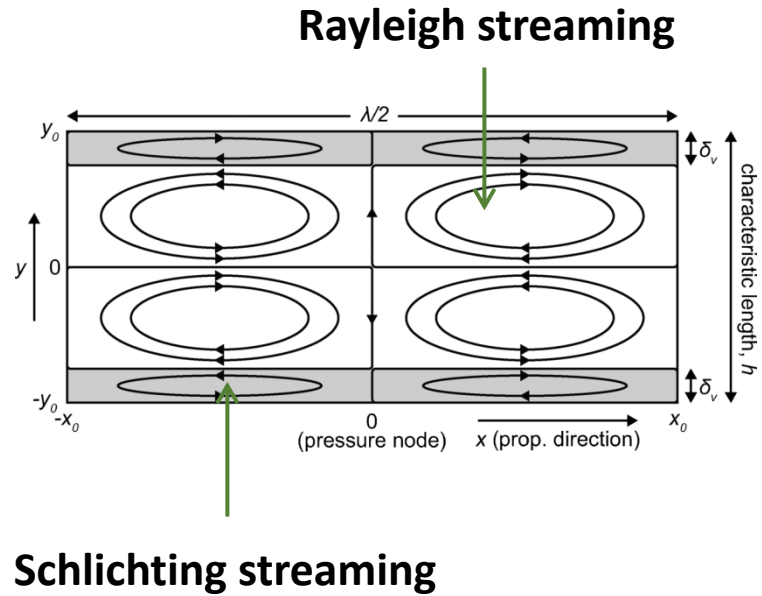




# Rayleigh streaming in a closed $\lambda/2$ resonator

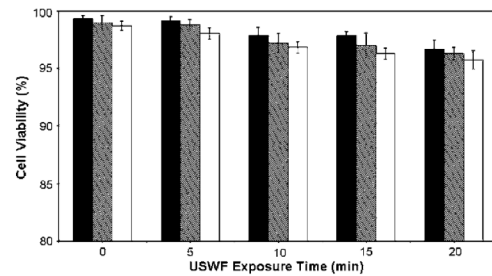
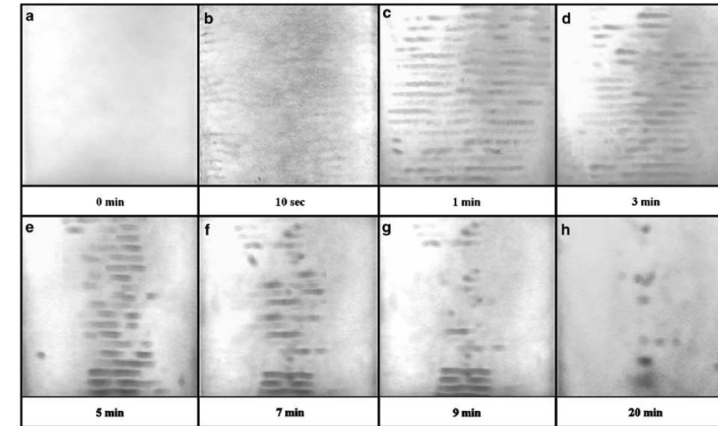
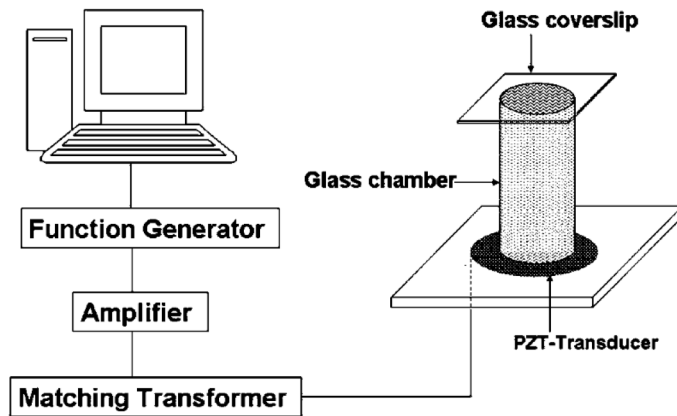


# Agglomeration of 10 $\mu\text{m}$ polymer beads

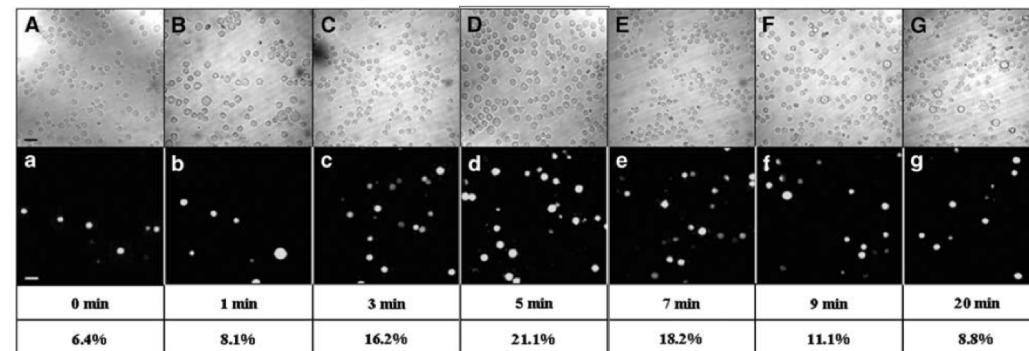


**Fig. 6** In-plane development of an aggregate of 10  $\mu\text{m}$  polymer beads at times (a) 0.2 s, (b) 5 s, (c) 15 s, (d) 60 s, (e) 130 s, and (f) 190 s. Once driven to the pressure nodal plane, the beads initially move away from the center of the field of view due to Rayleigh streaming (a–c). They interact off camera and return as compact mini-aggregates (d–e). The packing of the growing central aggregate adjusts to incorporate these merging mini-aggregates (f). The figure is taken from Spengler and Coakley.<sup>29</sup>

# Enhanced gene delivery with combination of radiation force and streaming



**Figure 3** Viability of K562 cells after exposure to USWF for various times. Followed by USWF exposure for 0, 5, 10, 15, and 20 min, cell viabilities of K562 cells were determined right away (■), after 24-h (▨), and after 48-h incubation (□), using a hemocytometer with the trypan-blue exclusion method. Each bar represents the mean of three independent experiments. Error bars are standard error of the mean cell viability ( $P < 0.05$ ).



Percentage of K562 cells with eGFP expression at various USWF exposure times.

What is the radiation force of retroviruses (100 nm size) vs. Radiation force on K562 leukemia cells (um range)?