

# NBE-E4310 - Biomedical Ultrasonics

## EXERCISE 5 (40p)

Independent/group work 21.3.2019 at 12-14; correct solutions 28.3.2019 at 12-14

*Submission: Please submit your responses via MyCourses as one zip file containing your responses in pdf and Matlab format.*

*The deadline for submitting your Exercise 5 responses is at 11:00 AM on Mar 28, 2019.*

---

### 1. Cavitation (11p)

Consider the differential equation proposed in the Exercise 4 task 1 and use same parameters.

- Calculate and plot the contribution of the pressure generated by the pulsating bubble to the total pressure field at a distance of  $15 \mu\text{m}$  from the centre of the bubble. Consider the bubble as a pulsating sphere source. (8p)
- Plot the amplitude spectrum of the total pressure signal. (3p)

The total pressure at a distance  $r$  from the centre of the bubble is given by the sum of the driving pressure and the pressure generated by the bubble.

$$p_{\text{tot}} = p_a + p_b$$

where  $p_b$  can be approximated as the pressure field generated by a pulsating sphere.

$$p_b = \frac{R}{r} v_r \rho_0 c_0 \frac{-ikR}{1 - ikR} e^{ik(r-R)}$$

where  $R$  is the radius of the bubble,  $r$  the observation point,  $v_r$  the bubble velocity.

```
%Parameters
c = 1500 ;           % speed of sound in water, m/s
rho = 998 ;         % water density, kg/m^3
```

```

sigma = 0.072 ; % surface tension, N/m
mu = 0.001; % shear viscosity, Pa*s
v0 = 0; % initial bubble boundary velocity, m/s
pinf = 101325; % ambient pressure, Pa
amp = 0.9e5; % pressure amplitude
gamma = 1.4; % ratio between the specific heat capacities
f = 500e3 ; % driving frequency, Hz
lambda = c/f; % wavelength, m
k = 2*pi/lambda; % wave vector, rad/m
omega = 2*pi*f; % angular frequency, rad/s
t_max = 65e-6; % maximum observation time
dt = 1/(100*f); % time step, us
R0 = 6.5e-6; % initial bubble radius

%Variables
syms R(t) pa(t)

Rt = diff(R,t); % first derivative of bubble radius, dR/dt
Rtt = diff(R,t,2); % second derivative of bubble radius, dR/dt
pa = amp*sin(2*pi*f*(t+R/c)); % time delayed driving pressure, Pa
p0 = pinf + 2*sigma/R0; % internal pressure of the bubble at equilibrium
pg = p0*(R0/R)^(3*gamma); % gas pressure in the interior of the bubble
pb = pg - 2*sigma/R - 4*mu*(Rt/R); % pressure on the liquid side of the bubble interface
pbt = diff(pb,t); % dpb/dt

% Define the differential equation
eqn1 = (1-Rt./c).*R.*Rtt + 3/2.*Rt.^2.*(1-Rt./(3.*c)) == (1+Rt./c).*1./rho.*(pb-pa-pinf) + R./

%Solve differential equation
[V] = odeToVectorField(eqn1);
M = matlabFunction(V,'vars', {'t','Y'});
sol = ode45(M,[0 t_max],[R0 v0]);

R = deval(sol,[0:dt:t_max],1); % bubble radius, m
v = deval(sol,[0:dt:t_max],2); % bubble velocity, m/s
a = [0 diff(v)/dt]; % bubble acceleration, m/s

% Pressure generated by the bubble
r = 15e-6; % distance from the bubble centre, m
pb = R/r.*max(abs(v)).*rho.*c.*(-i.*k.*R)./(1-i.*k.*R).*exp(i.*k.*(r-R)-i.*omega.*[0:dt:t_max]);
pa = amp*sin(2*pi*f*[0:dt:t_max] + r/c); % time delayed driving pressure, Pa
p_tot = real(pb) + pa; % total pressure, Pa

% Plot

figure

subplot(211)
plot([0:dt:t_max]*1e6, p_tot*1e-6)
xlabel('Time (\mus)')
ylabel('Pressure (MPa)')
title('Total pressure field')
% xlim([30 50])

```

```

% ylim([-0.4 0.4])

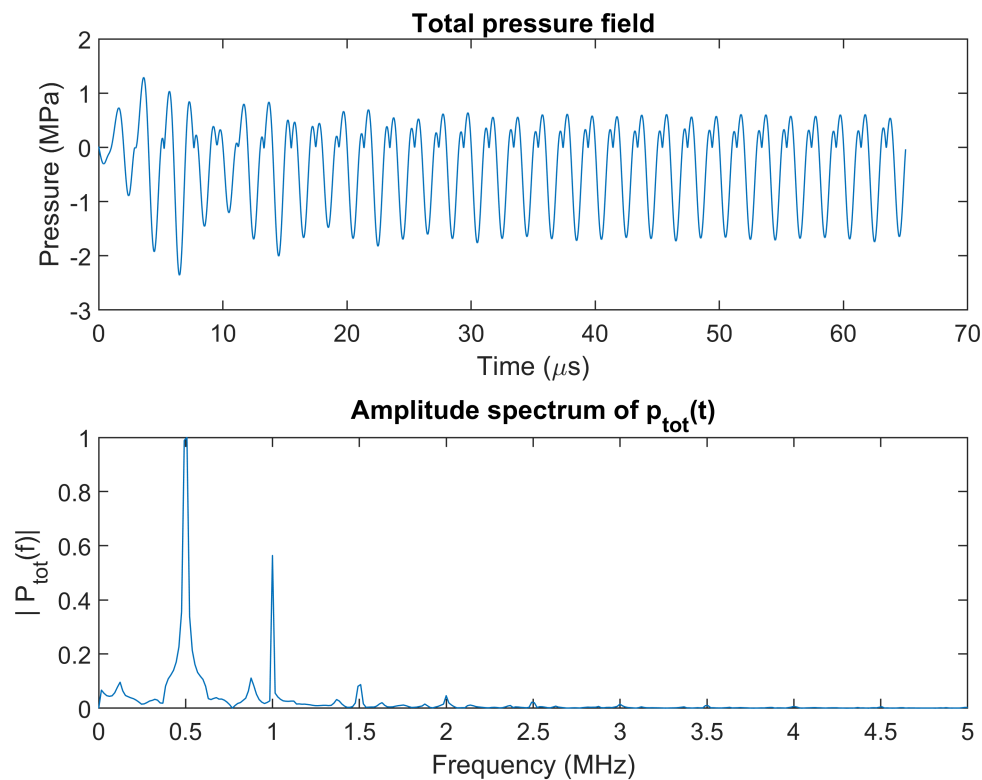
subplot(212)
Fs = 1/dt;           % Sampling frequency
T = t_max;          % Sampling period
L = length(R);      % Length of signal
t = (0:L-1)*T;      % Time vector

X = p_tot-mean(p_tot);

Y = fft(X);
P2 = abs(Y/L);
P1 = P2(1:(L/2)+1);
P1(2:end-1) = 2*P1(2:end-1);

f = Fs*(0:(L/2))/L/1e6;
plot(f,P1/max(P1))
title('Amplitude spectrum of p_{tot}(t)')
xlabel('Frequency (MHz)')
ylabel('| P_{tot}(f) |')
xlim([0 5])

```



## 2. Thermal Dose 1 (9p)

Calculate how long it takes to reach tissue damage ( $30 < TD_{43} < 240$ ) and tissue necrosis ( $TD_{43} > 240$ ) in the following cases:

a)  $T_1 = 42.5 \text{ }^\circ\text{C}$  (3p)

```

T = 42.5; % Costant temperature, °C
tissue_dmg_tsh = 30*60; % Equivalent time at 43 °C for tissue damage, s
necrosis_tsh = 240*60; % Equivalent time at 43 °C for necrosis, s
R = 0.25;

syms t

eqn1 = tissue_dmg_tsh == int(R^(43-T),t,0,t);
eqn2 = necrosis_tsh == int(R^(43-T),t,0,t);

t_tissue_dmg = double(solve(eqn1,t)); % Time for tissue damage at T, s
t_necrosis = double(solve(eqn2,t)); % Time for necrosis at T, s

```

$$t_{\text{tissue damage}} = 1h$$

$$t_{\text{necrosis}} = 8h$$

b)  $T_2 = 54 \text{ }^\circ\text{C}$  (3p)

```

T = 54; % Costant temperature, °C
R = 0.5;

syms t

eqn1 = tissue_dmg_tsh == int(R^(43-T),t,0,t);
eqn2 = necrosis_tsh == int(R^(43-T),t,0,t);

t_tissue_dmg = double(solve(eqn1,t)); % Time for tissue damage at T, s
t_necrosis = double(solve(eqn2,t)); % Time for necrosis at T, s

```

$$t_{\text{tissue damage}} = 0.9s$$

$$t_{\text{necrosis}} = 7s$$

c)  $T_3 = 80 \text{ }^\circ\text{C}$  (3p)

```

T = 80; % Costant temperature, °C
R = 0.5;

syms t

```

```

eqn1 = tissue_dmg_tsh == int(R^(43-T),t,0,t);
eqn2 = necrosis_tsh == int(R^(43-T),t,0,t);

t_tissue_dmg = double(solve(eqn1,t));      % Time for tissue damage at T, s
t_necrosis = double(solve(eqn2,t));      % Time for necrosis at T, s

```

$$t_{\text{tissue damage}} = 13 \text{ ns}$$

$$t_{\text{necrosis}} = 100 \mu\text{s}$$

### 3. Thermal Dose 2 (10p)

Calculate how long it takes to reach tissue damage ( $30 < \text{TD}_{43} < 240$ ) and tissue necrosis ( $\text{TD}_{43} > 240$ ) in the following cases:

a)  $T_1(t) = 70(1 - e^{-t/10})$  °C (5p)

```

R = 0.5 ;

syms t
T1(t) = 70*(1-exp(-t/10));

eqn1 = tissue_dmg_tsh == int(R^(43-T1(t)),t,0,t);
eqn2 = necrosis_tsh == int(R^(43-T1(t)),t,0,t);

t_tissue_dmg = double(solve(eqn1,t));      % Time for tissue damage at T, s
t_necrosis = double(solve(eqn2,t));      % Time for necrosis at T, s

```

$$t_{\text{tissue damage}} = 14 \text{ s}$$

$$t_{\text{necrosis}} = 16.7 \text{ s}$$

b)  $T_2(t) = 55(1 - e^{-t/15})$  °C (5p)

```

R = 0.5 ;

syms t
T1(t) = 55*(1-exp(-t/15));

eqn1 = tissue_dmg_tsh == int(R^(43-T1(t)),t,0,t);
eqn2 = necrosis_tsh == int(R^(43-T1(t)),t,0,t);

t_tissue_dmg = double(solve(eqn1,t));      % Time for tissue damage at T, s
t_necrosis = double(solve(eqn2,t));      % Time for necrosis at T, s

```

$$t_{\text{tissue damage}} = 41s$$

$$t_{\text{necrosis}} = 55s$$

## 4. Biomedical applications (10p)

a) Define the parameters that should be used in order to achieve histotripsy at 1 MHz without inducing thermal damage in tissue. (5p)

In order to obtain tissue homogenisation, the mechanical index should be high enough to produce cavitation. If we consider a MI = 3 then:

$$\text{PNP} = \text{MI} \sqrt{f} = 3 \text{ MPa}$$

Assuming that the signal is sinusoidal, with  $\text{PNP} = \text{PPP} = p_0$ , the  $I_{\text{spta}}$  is given by:

$$I_{\text{spta}} = \text{DC} I_{\text{sppa}} = \frac{I_0}{2} \text{DC}$$

where  $I_0 = \frac{\text{PNP}^2}{\rho c}$  and PRP has to be defined.

Thermal damage should be also avoided, which means:

$$\text{TD}_{43} = \int_0^t R^{43-T(t)} dt < 30 \text{ min}$$

From the Pennes' Bioheat Transfer Equation one can obtain the relation between the rate of temperature change and the the ultrasound power

deposition per unit volume:

$$\rho_t c_t \frac{dT}{dt} = 2\alpha I_{\text{spta}}$$

where  $\rho_t$  is the tissue density,  $c_p$  is the tissue specific heat capacity and  $\alpha$  is the absorption coefficient. The time variation of the temperature is given by:

$$T_2(t) = T_1 + 2\alpha \frac{I_{\text{spta}}}{\rho_t c_t} t$$

By including the temperature expression into the thermal dose expression and integrating we obtain:

$$\text{TD}_{43} = -\frac{\rho_t c_t}{\alpha I_0 \text{DC}} \frac{R^{43-T_1 - \alpha \frac{I_0 \text{DC}}{\rho_t c_t} t}}{\ln(R)} < 30 \text{ min}$$

which gives the general formula to calculate what the DC should for a specific signal duration in order not to cause thermal damage in tissue.

If we consider a signal duration of 1h, then  $DC < 0.007\%$ .

```

alpha = 0.1e-2 ;           % Absorption coefficient in liver, 1/m (Ultrasonic absorption)
rho = 1079 ;               % Liver density, kg/m^3
c_p = 3540 ;               % heat capacity of liver
c = 1600 ;                 % speed of sound in liver, m/s
f = 1e6 ;                  % US frequency, Hz
TD_43 = 30*60;            % thermal dose threshold, s
R = 0.25 ;                 %
T1 = 37 ;                  % initial temperature, °C
PNP = 3e6 ;                % Peak negative pressure, Pa
I0 = PNP^2/rho/c;         % acoustic intensity peak, W/m^2
t = 3600;                  % signal duration, s

syms DC

eqn = -rho*c_p/(alpha * I0 *DC) * 1/log(R)*R^(43 - T1 - alpha * I0 * DC/(rho*c_p)*t) == TD_43;

DC = double(solve(eqn, DC));

```

b) Define the parameters that should be used in order to achieve thermal ablation at 1 MHz without inducing cavitation. (5p)

In order to obtain tissue thermal ablation, the thermal dose has to be greater than  $240 \text{ CEM}_{43}$ . The mechanical index instead has to be lower than 0.5 to avoid cavitation. The peak negative pressure should be:

$$\text{PNP} = \sqrt{f} * \text{MI} = 500 \text{ kPa}$$

In this case  $DC > 4\%$ .

```

alpha = 0.1e-2 ;           % Absorption coefficient in liver, 1/m (Ultrasonic absorption)
rho = 1079 ;               % Liver density, kg/m^3
c_p = 3540 ;               % heat capacity of liver
c = 1600 ;                 % speed of sound in liver, m/s
f = 1e6 ;                  % US frequency, Hz
TD_43 = 240*60;           % thermal dose threshold, s
R = 0.5 ;                  %
T1 = 37 ;                  % initial temperature, °C
PNP = 500e3 ;              % Peak negative pressure, Pa
I0 = PNP^2/rho/c;         % acoustic intensity peak, W/m^2
t = 3600;                  % signal duration, s

syms DC

eqn = -rho*c_p/(alpha * I0 *DC) * 1/log(R)*R^(43 - T1 - alpha * I0 * DC/(rho*c_p)*t) == TD_43;

```

```
DC = double(solve(eqn, DC));
```